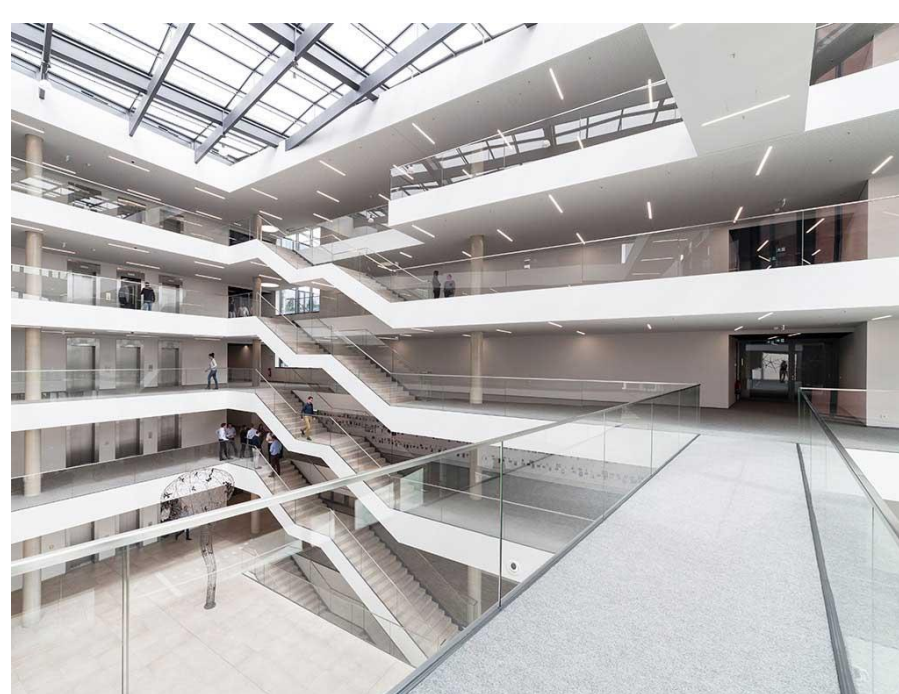
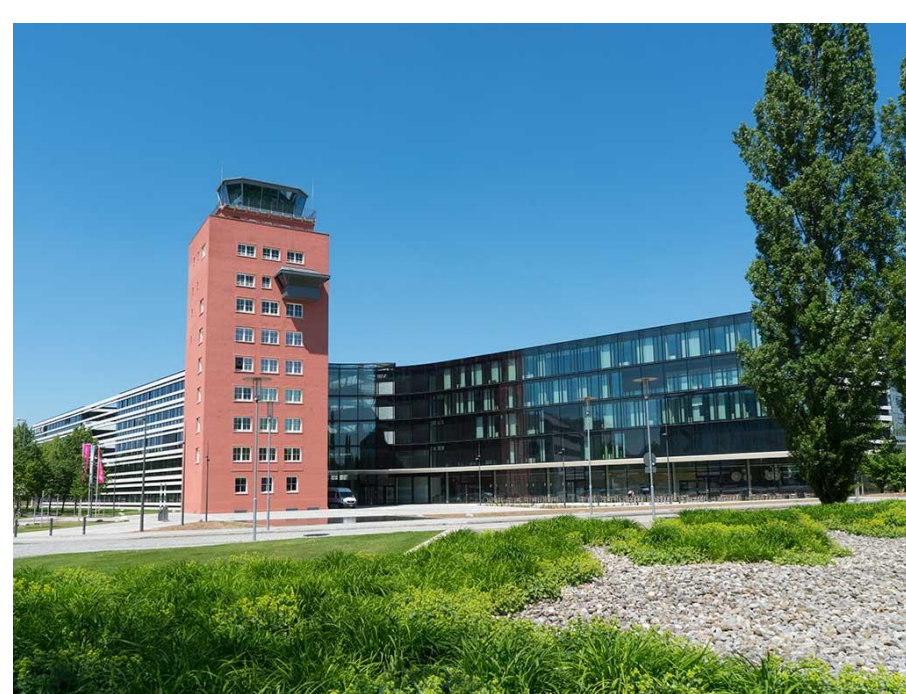


15 novembre 2017

# IMAGING EVOLUTO E PRECISIONE IN RADIOCHIRURGIA CEREBRALE

ING. PIER PAOLO RAGUZZI  
SALES MANAGER RT  
BRAINLAB ITALIA SRL



**BRAINLAB - CORPORATE OVERVIEW**

- Founded in Munich, Germany in 1989
- Privately held since inception
- Over 1300 employees in 17 offices worldwide
- More than 290 R&D engineers
- More than 5,000 systems installed



# RadioChirurgia Stereotassica Brain

## Meningiomas of the anterior skull base

Optic neuropathy

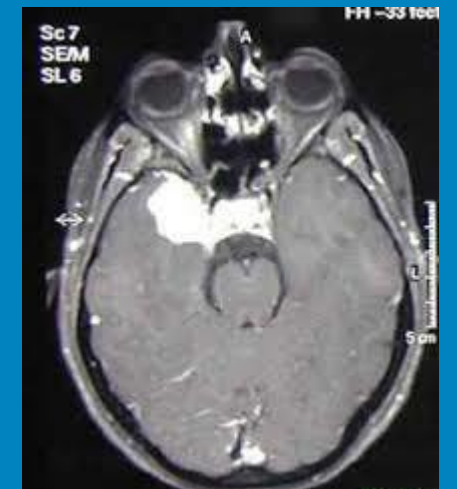
### Traditional limits

Doses  $< 8$  Gy

Tumour - AOP distance  $> 3$ mm

Stafford SL et al. A study on the radiation tolerance of the optic nerves and chiasm after stereotactic radiosurgery. *Int J Radiat Oncol Biol Phys* 2003

Tishler RB et al. Tolerance of cranial nerves of the cavernous sinus to radiosurgery. *Int J Radiat Oncol Biol Phys* 1993



Courtesy of

# Periopic Meningiomas

## single-session Radiosurgery

Hasegawa T et al. 2010 Tolerance of the optic apparatus in single-fraction irradiation using stereotactic radiosurgery: Evaluation in 100 patients with craniopharyngioma.

**14 Gy**

Leavitt JA et al. 2013 Long-term evaluation of radiation-induced optic neuropathy after single-fraction stereotactic radiosurgery

**12 Gy**

Pollock BE et al. 2014 Dose-Volume Analysis of Radiation-Induced Optic Neuropathy After Single-Fraction Stereotactic Radiosurgery

**12 Gy**

# Periopic Meningiomas

## multisession Radiosurgery

Multisession radiosurgery for optic nerve sheath meningiomas, an effective option:  
preliminary results of a single-center experience

Marchetti M, Bianchi S, Milanese I, Bergantin A, Bianchi L, Broggi G, Fariselli L.

**Neurosurgery. 2011**

25Gy/5fr

Staged image guided robotic radiosurgery for optic nerve sheath meningiomas. Romanelli P,  
Bianchi L, Muacevic A, Beltramo G.

**Comput Aided Surg. 2011**

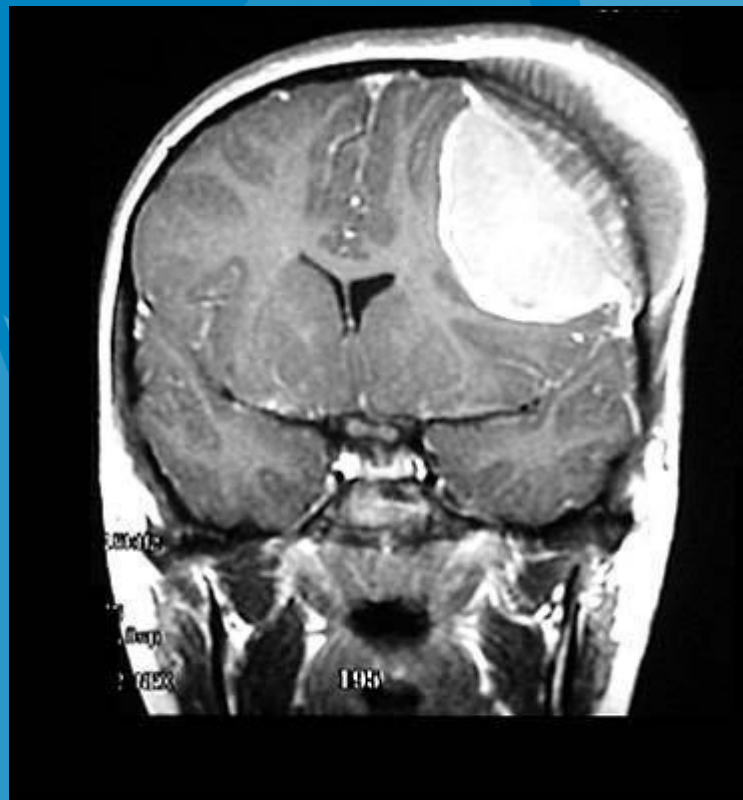
20Gy/4fr

Diagnosis and management of optic nerve sheath meningiomas

Shapey J, Sabin HI, Danesh-Meyer HV, Kaye AH

**J Clin Neurosci. 2013**

20Gy/4fr



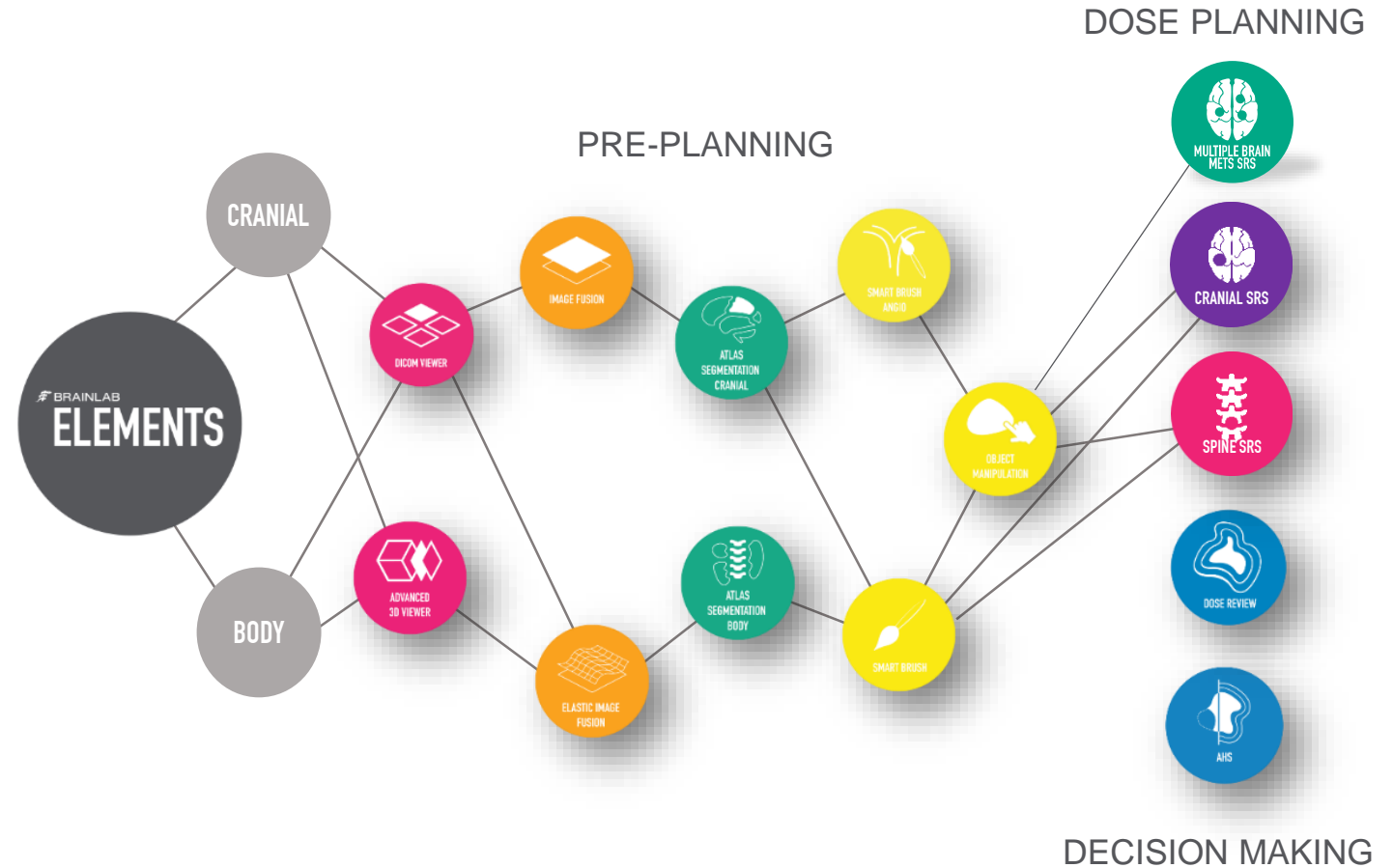
**Fig. 1: RMN di un paziente con Meningioma**



# BRAINLAB ELEMENTS

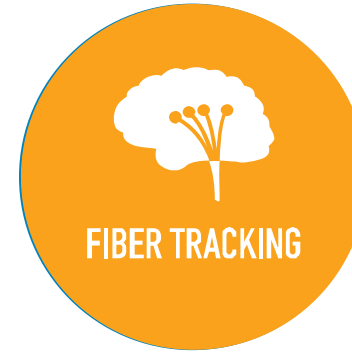
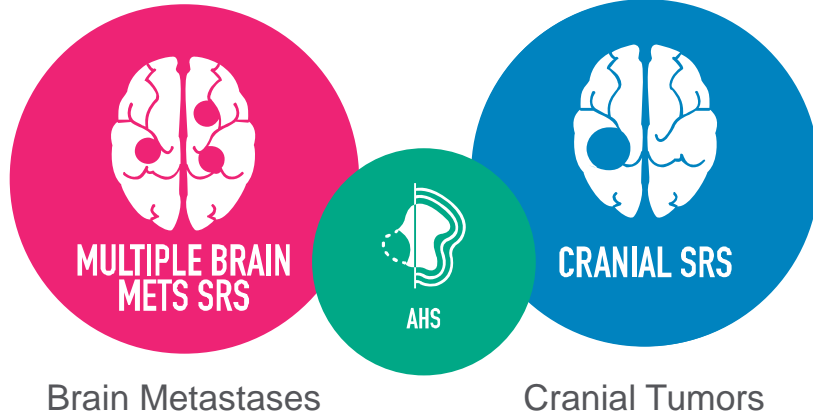
## Concept

- Moduli software per obiettivi clinici specifici
- Vantaggio della **modularita'** al fine di costruire e customizzare i vari workflow
- **Algoritmi intelligenti** e ambiente utente intuitivo
- Al Servizio di piu' specialita' cliniche dalla **Radioterapia alla Neurochirurgia**



# BRAINLAB ELEMENTS

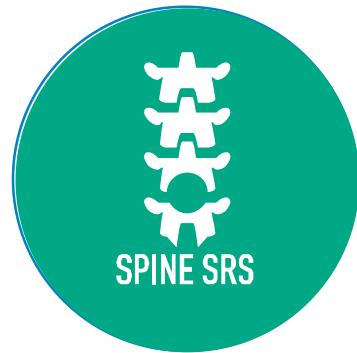
Software per indicazioni specifiche



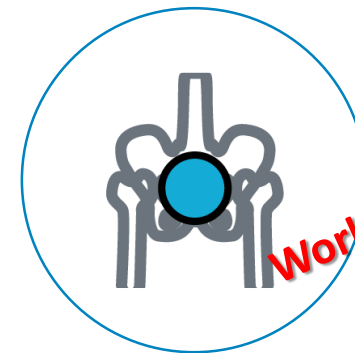
Functional Indications



Vascular Malformations



Spine Metastases



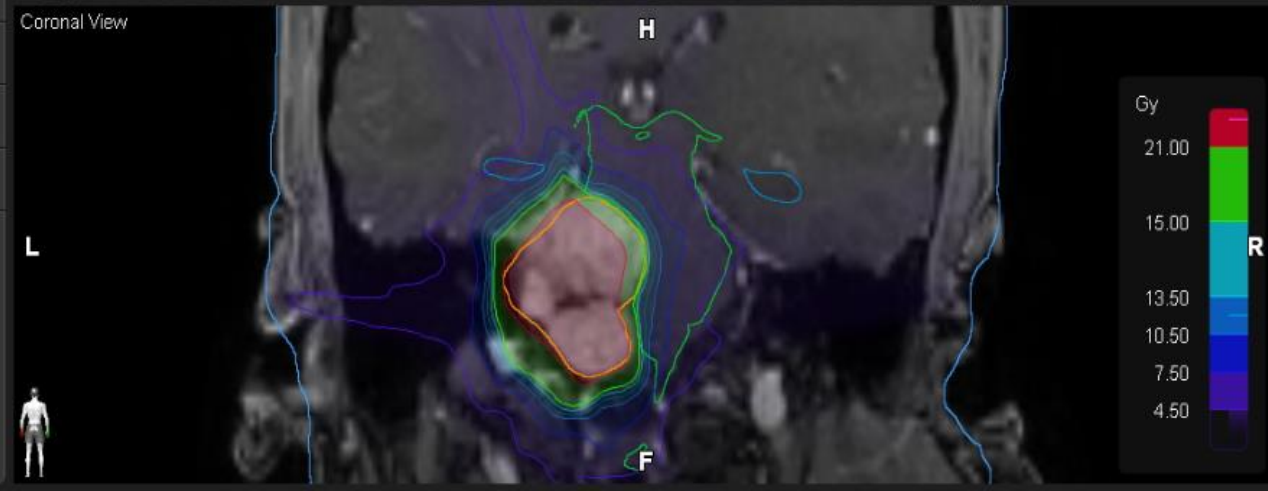
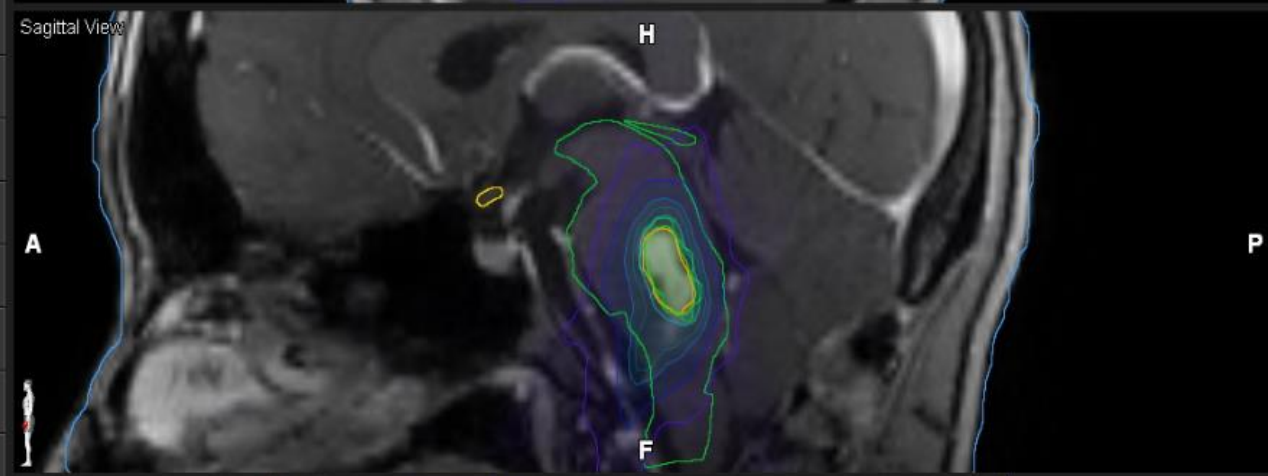
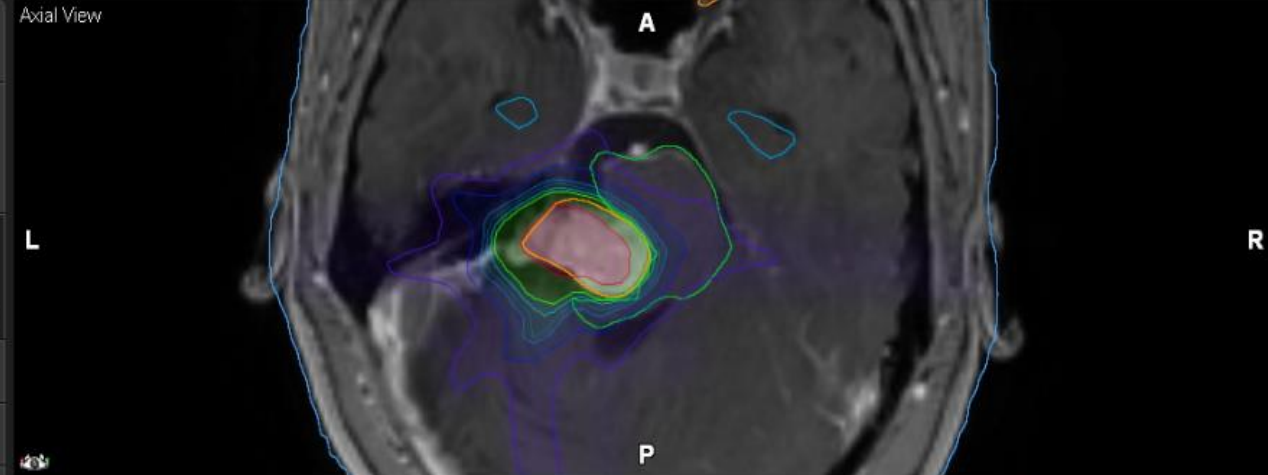
Prostate



Lung



Benign Meningioma		cf-SRT 30x1.8Gy	hf-SRS 5x5Gy	sf-SRS 1x15Gy
test	Volume Coverage (%) Conformity Index (CI)	99% (99%) 1.2 (1.6)	99% (99%) 1.1 (1.5)	99% (99%) 1.7 (1.4)
Brainstem		19 Gy (45 Gy) 57 Gy (54 Gy)	9 Gy (12 Gy) 26 Gy (25 Gy)	5 Gy (8 Gy) 18 Gy (12 Gy)
<input checked="" type="checkbox"/> D <sub>50</sub>	<input checked="" type="checkbox"/> Max	D <sub>50</sub> (Gy) Max Dose (Gy)		
Optic Tract Left				
Chiasm				
Cochlea Left				
Cochlea Right				
Eye Left				
Eye Right				
Lens Left				
Lens Right				
Optic Nerve Left				
Optic Nerve Right				
Optic Tract Right				
Hippocampus Left				
Hippocampus Right				



DEMO, Large benign acou...  
AHSA 02-2014/08

Adaptive Hybrid Surgery  
Analysis

Scroll Zoom  
Pan Windowing

Dose

Dose Off  
Dose Distribution

Highlight 4.50 Gy

Back Done

BRAINLAB

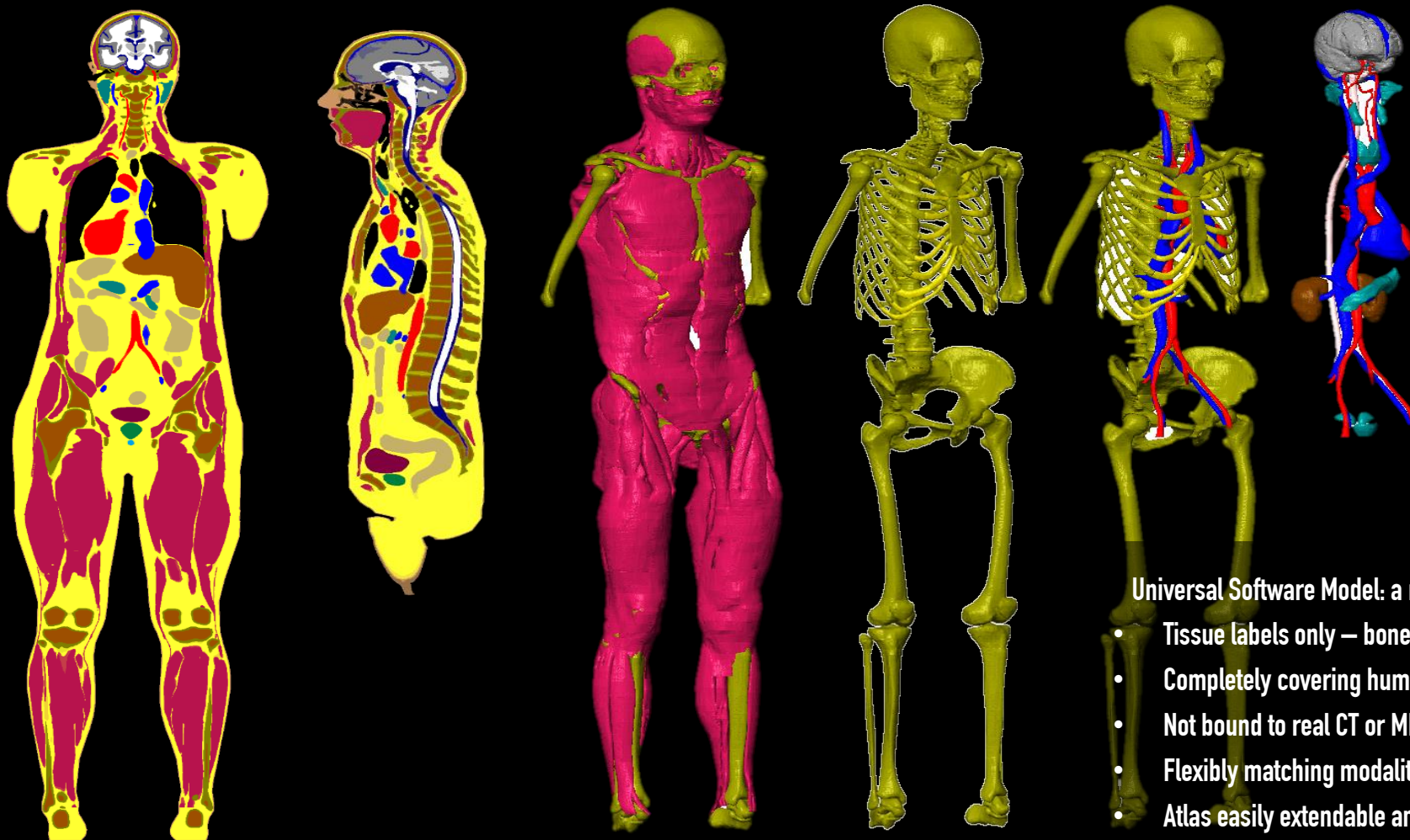
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**BRAINLAB ELEMENTS**

**ANATOMICAL MAPPING**



# UNIVERSAL SOFTWARE MODEL

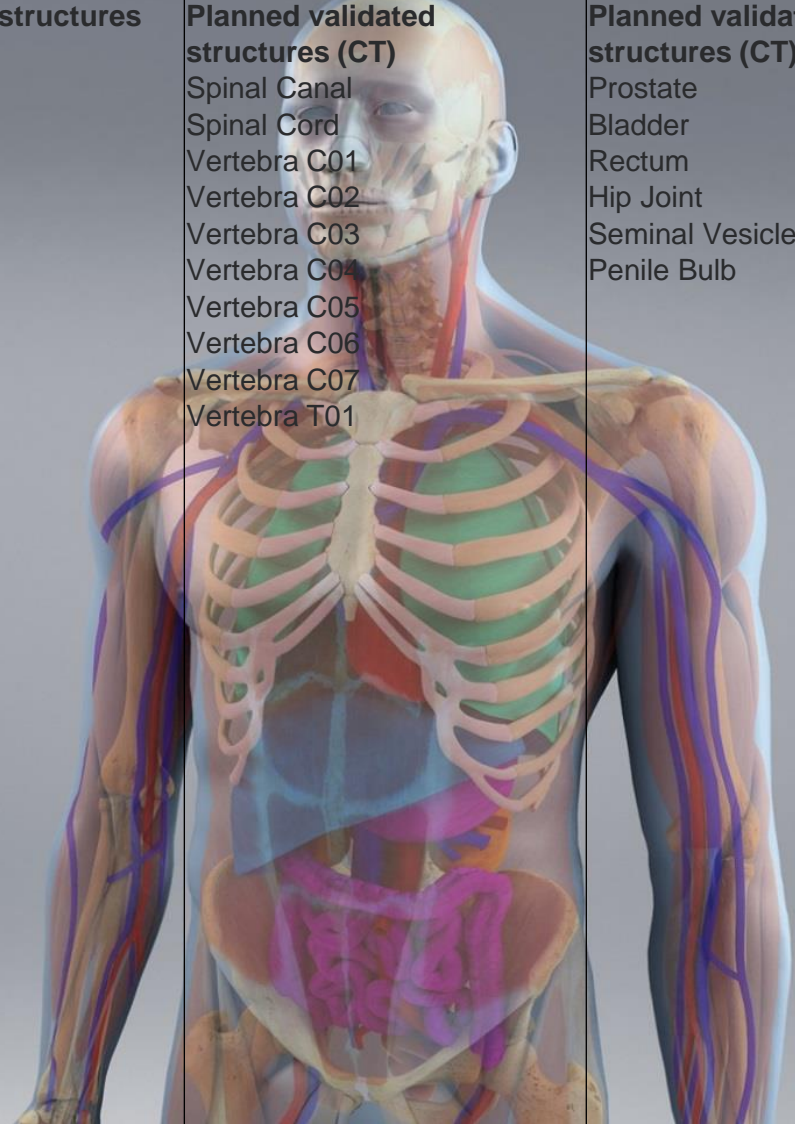


Universal Software Model: a new segmentation approach

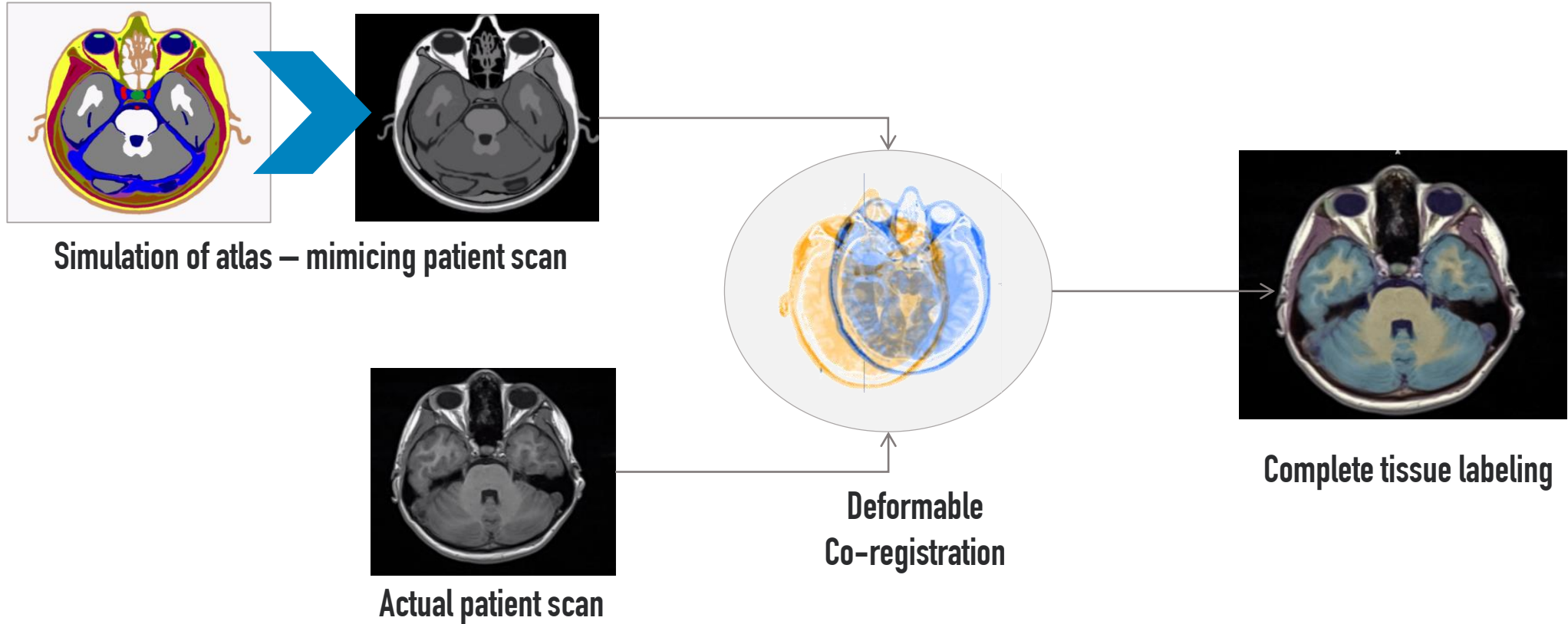
- Tissue labels only – bone, fat, muscles, organs
- Completely covering human body, not just critical structures
- Not bound to real CT or MR scans
- Flexibly matching modality diversity
- Atlas easily extendable and refinable
- Better & more robust registrations

# UNIVERSAL SOFTWARE MODEL

Elements Segmentation Cranial	Elements Segmentation H&N	Elements Segmentation Thoracic	Elements Segmentation Spine	Elements Segmentation Pelvic
<b>Planned validated structures (MR)</b> Brainstem Optic Nerve Chiasm Optic Tract Eyes Lens Whole Brain Cochlea Hippocampus Cerebellum Temporal Lobe Cerebrum White Matter Gray Matter Hypothalamus Putamen Corpus Callosum Pineal Gland CSF Brain Caudatus Ventricles Geniculate Body Globus Pallidus Pituitary Gland Nucleus Caudatus Capsula Externa Capsula Interna Amygdala	<b>Planned validated structures (CT)</b> Brainstem Cricoid Cartilage Hyoid Cochlea Eye Lens Lymph Level 1A Lymph Level 1B Lymph Level 2 Lymph Level 3 Lymph Level 4 Lymph Level 5 Lymph Level 6 Lymph Node RCL Lymph Node RP Lymph Node RST Parotid Gland Sternocleidomastoid Muscle Submandibular Gland Mandible Thyroid Cartilage Thyroid Gland	<b>Planned validated structures (CT)</b> Aorta Vena Cava Inferior Clavicle Heart Kidney Lung Liver Esophagus Ribs Sternum Manubrium Trachea	<b>Planned validated structures (CT)</b> Spinal Canal Spinal Cord Vertebra C01 Vertebra C02 Vertebra C03 Vertebra C04 Vertebra C05 Vertebra C06 Vertebra C07 Vertebra T01	<b>Planned validated structures (CT)</b> Prostate Bladder Rectum Hip Joint Seminal Vesicle Penile Bulb

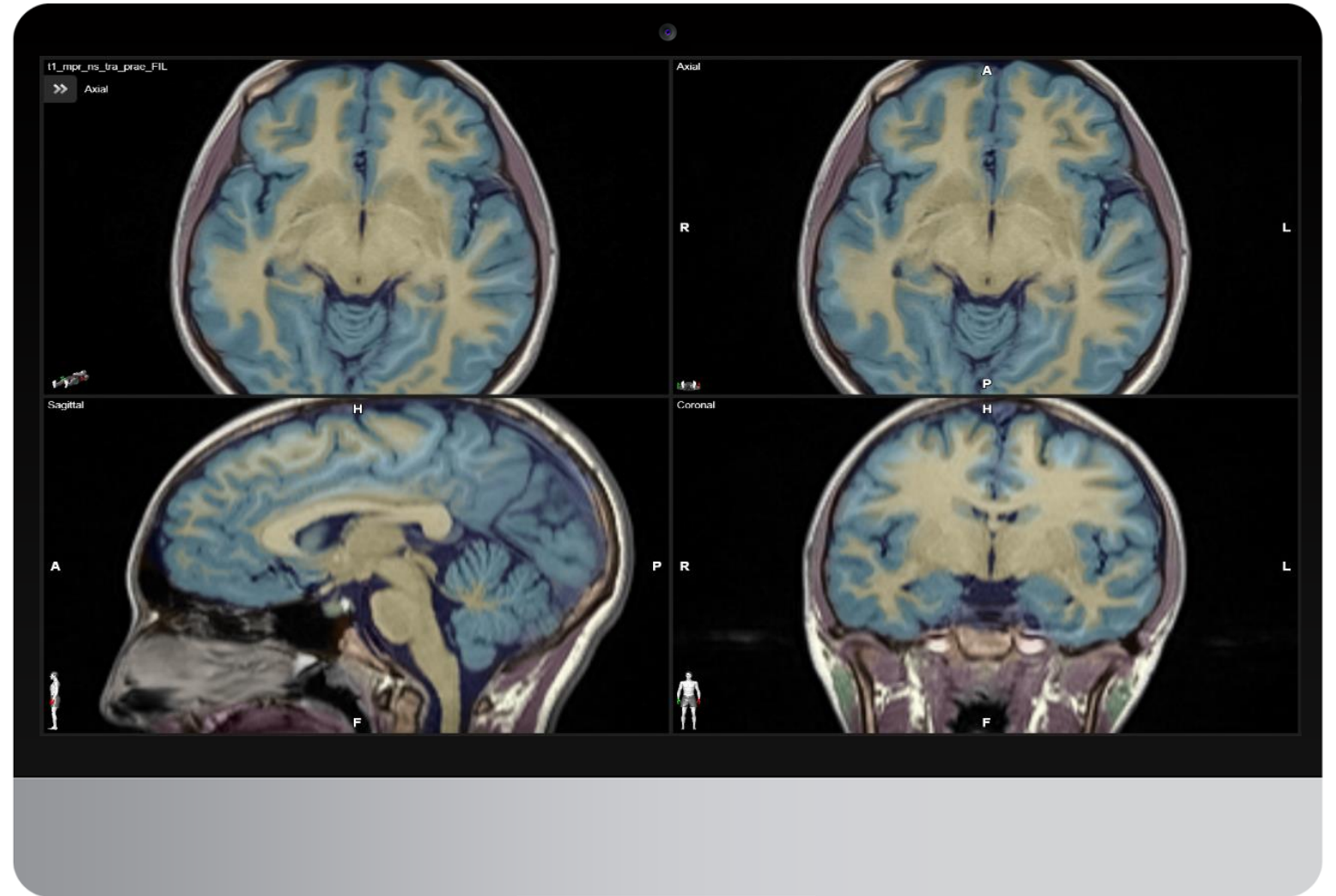


# ANATOMICAL MAPPING



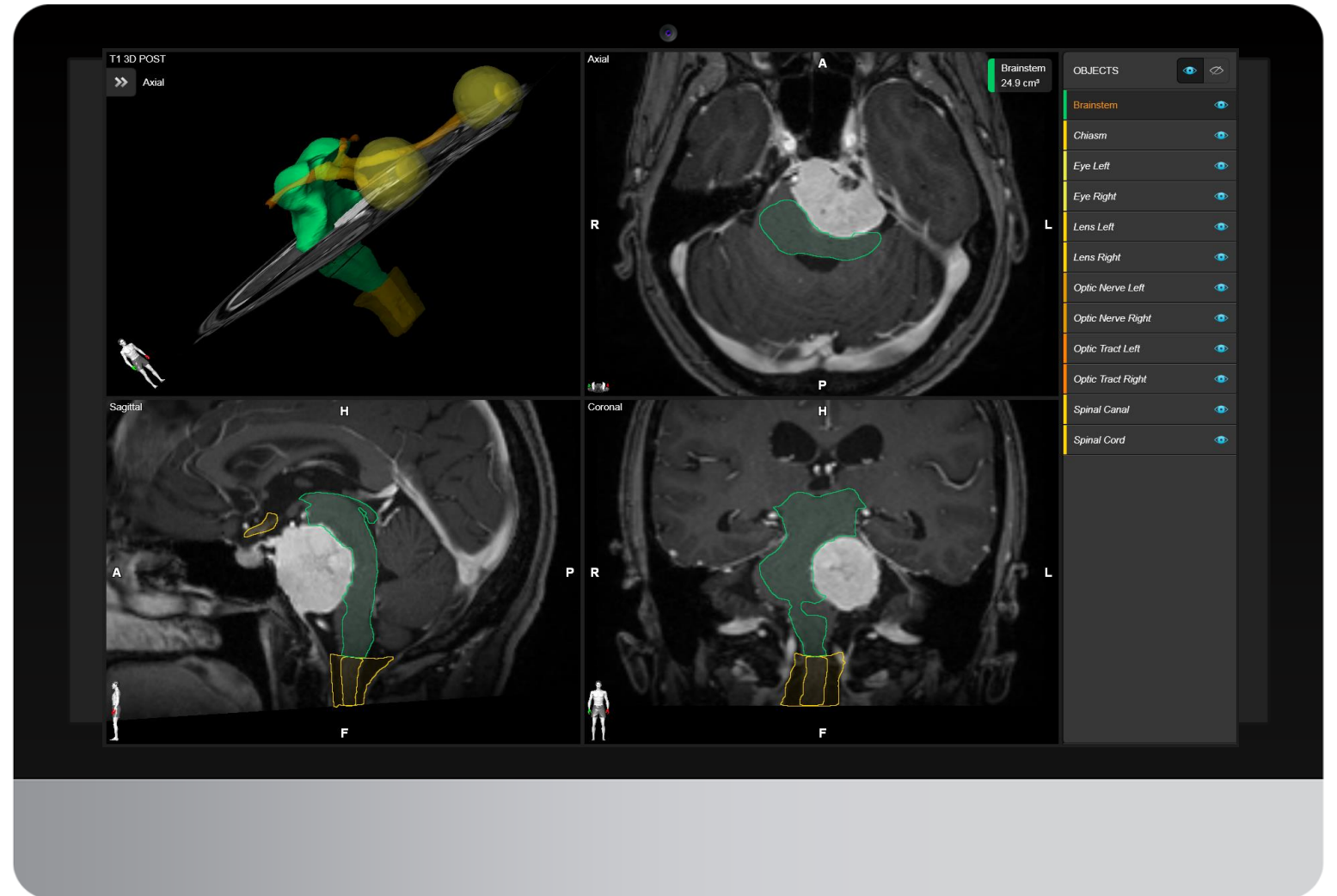
# ANATOMICAL MAPPING

- Basato su un modello tissutale universale completamente nuovo
- Adattabile dinamicamente e indipendente dalla modalita' di acquisizione
- Classificazione completa del tessuto in tutto il corpo
- Vengono considerate sequenze MR multiple di uno studio per eseguire la registrazione
- Visualizzazione completa della registrazione sottostante

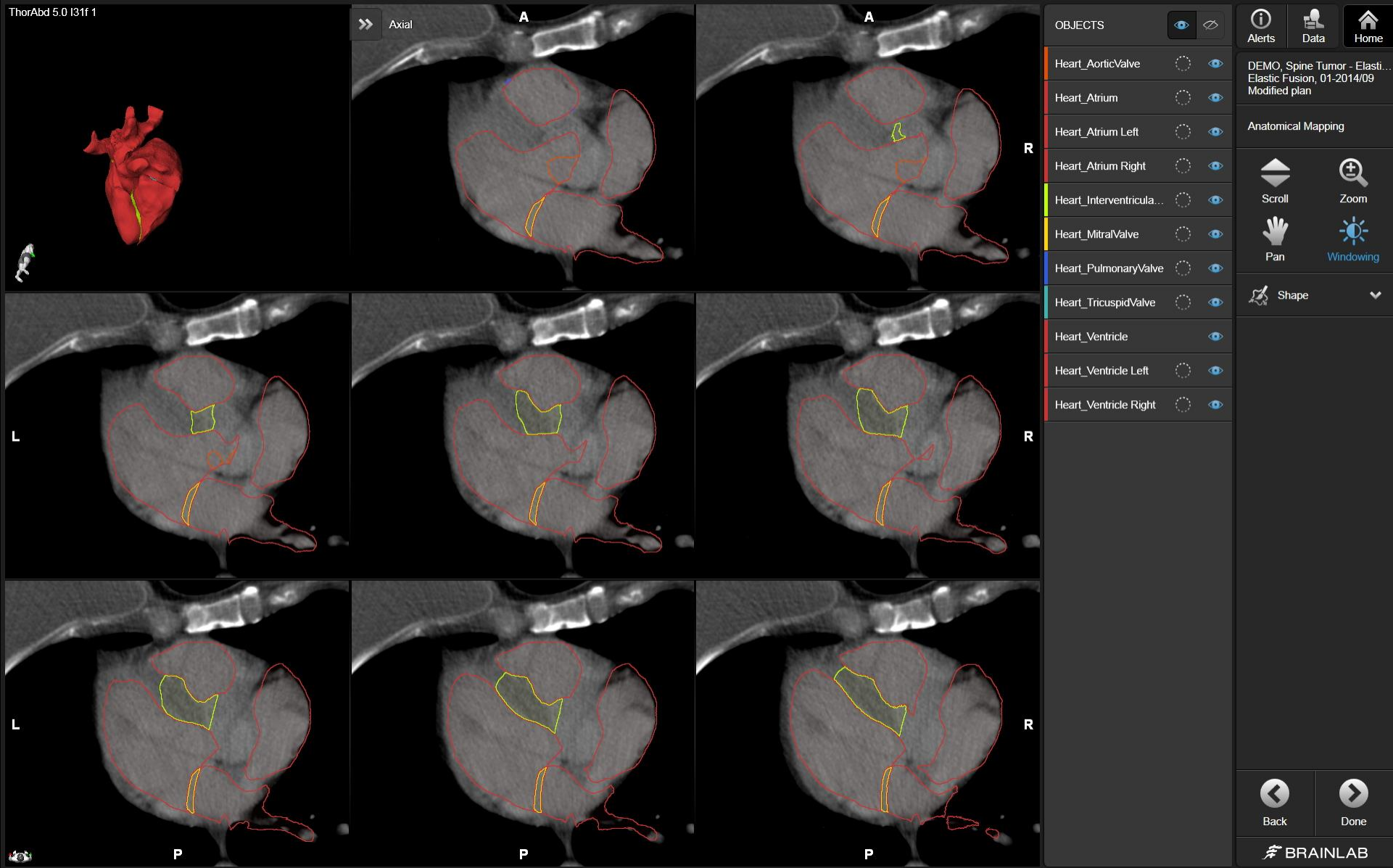


# ANATOMICAL MAPPING

- Basato su un modello tissutale universale completamente nuovo
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- Classificazione completa del tessuto in tutto il corpo
- Vengono considerate sequenze MR multiple di uno studio per eseguire la registrazione
- Visualizzazione completa della registrazione sottostante







ThorAbd 5.0 I31f 1

Axial reformatted range  
Slice distance 1.2 mm

A

Heart\_PulmonaryValve  
1.52 cm<sup>2</sup>

OBJECTS

- Heart\_AorticValve
- Heart\_Atrium
- Heart\_Atrium Left
- Heart\_Atrium Right
- Heart\_Interventricula...
- Heart\_MitralValve
- Heart\_PulmonaryValve
- Heart\_TricuspidValve
- Heart\_Ventricle
- Heart\_Ventricle Left
- Heart\_Ventricle Right

Alerts Data Home

DEMO, Spine Tumor - Elasti...  
Elastic Fusion, 01-2014/09  
Modified plan

Anatomical Mapping

Scroll Zoom

Pan Windowing

Shape

Back Done

BRAINLAB

# BRAINLAB ELEMENTS

# IMAGE FUSION

- CRANIAL DISTORTION CORRECTION
- SPINE CURVATURE CORRECTION

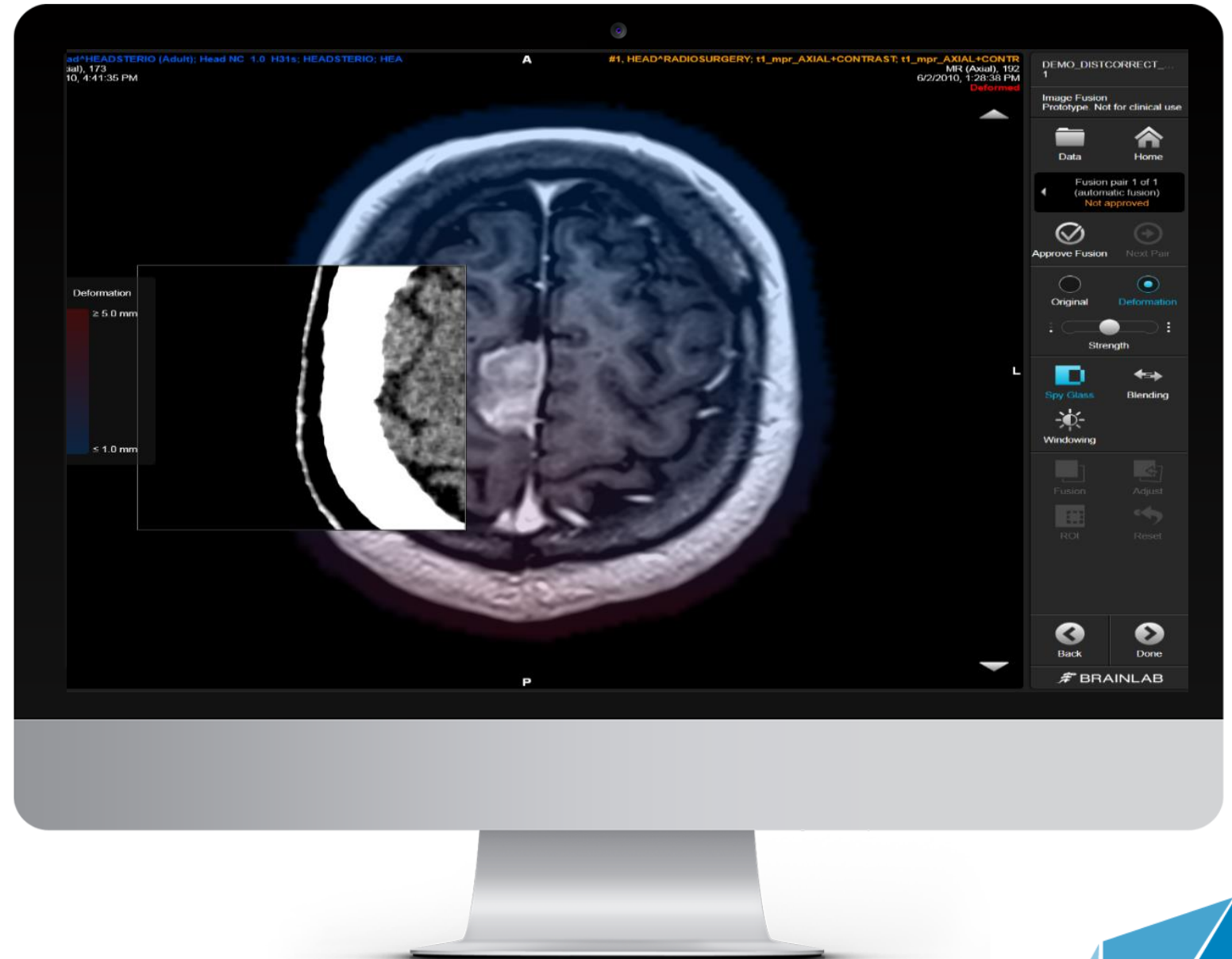
# CRANIAL DISTORTION CORRECTION

## IMAGE FUSION con CRANIAL DISTORTION CORRECTION

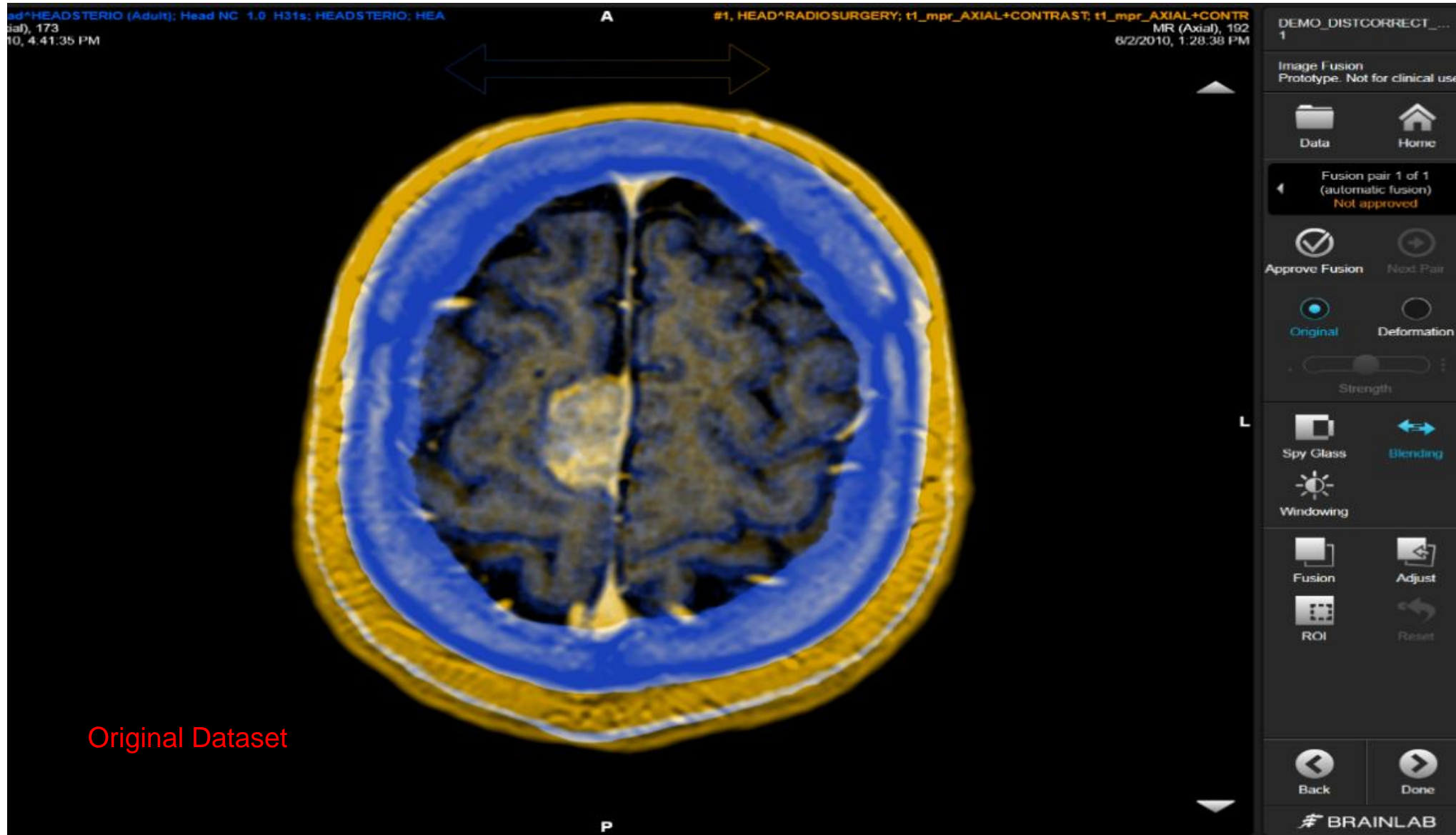
- Co-registrazione multi-modale deformabile: Cranial MR  $\leftrightarrow$  planning CT
- Permette il contornamento del tumore basato su MR utilizzando il data set corretto con dalla distorsione.
- Nessuna necessita' di operare una fusion locale con ROI

## QUALITY ASSURANCE

- Valutazioni della posizione e grandezza delle distorsioni
- Panoramica rapida su quale MR è la scelta migliore per la definizione precisa del bersaglio
- Facile confronto dei risultati corretti rispetto alla versione rigida o distorta.

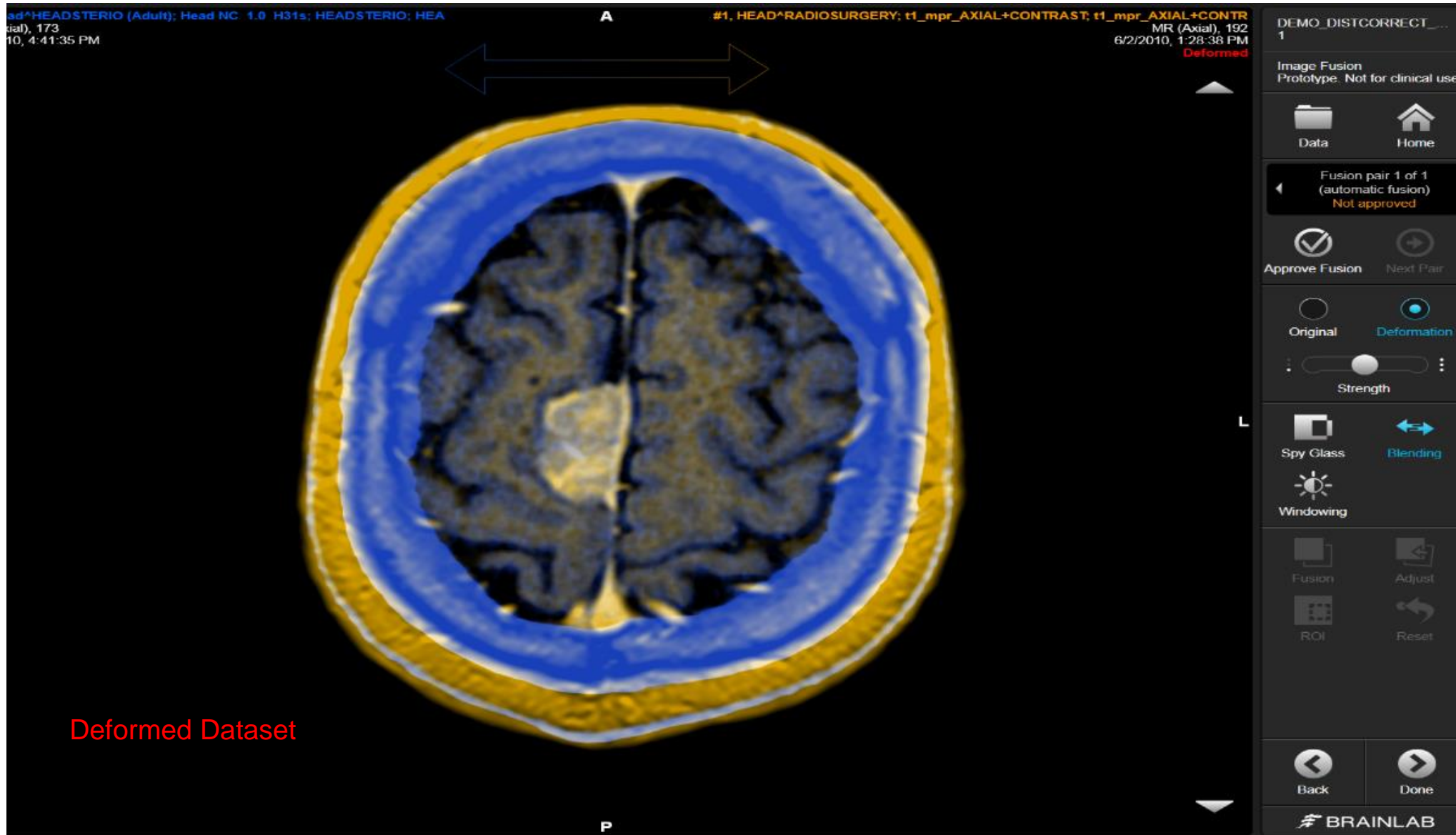


# CRANIAL DISTORTION CORRECTION



Original Dataset

# CRANIAL DISTORTION CORRECTION



# CRANIAL DISTORTION CORRECTION

ad^HEADSTERIO (Adult); Head NC 1.0 H31s; HEADSTERIO; HEA  
ial), 173  
10, 4:41:35 PM

#1, HEAD^RADIOSURGERY; t1\_mpr\_AXIAL+CONTRAST; t1\_mpr\_AXIAL+CONTR  
MR (Axial), 192  
6/2/2010, 1:28:38 PM  
Deformed

DEMO\_DISTCORRECT\_...  
1

Image Fusion  
Prototype. Not for clinical use

Data Home

Fusion pair 1 of 1  
(automatic fusion)  
Not approved

Approve Fusion Next Pair

Original Deformation

Strength

Spy Glass Blending

Windowing

Fusion Adjust  
ROI Reset

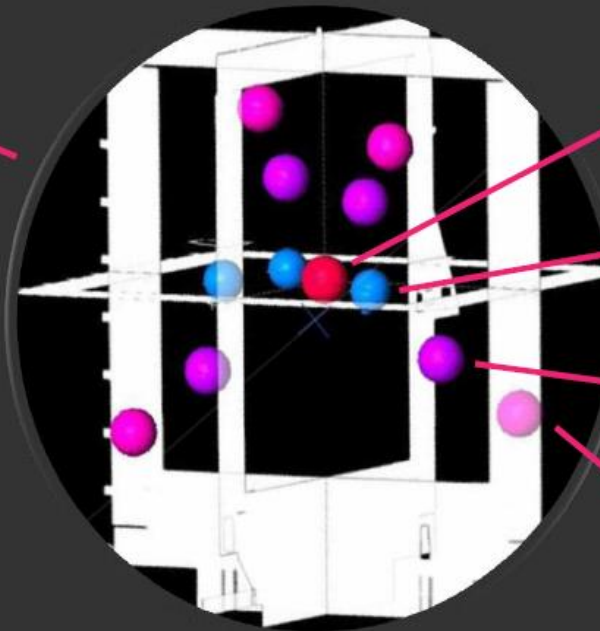
Back Done

BRAINLAB

Deformation grid enables visualization of local deformations

## EXACTRAC POSITIONING ACCURACY FOR MULTIPLE TARGETS IN INTRACRANIAL IMAGE-GUIDED RADIATION THERAPY: A PHANTOM STUDY

**DEDICATED PHANTOM**  
The phantom is positioned with ExacTrac and the positioning is evaluated with CBCT. The effect of rotations as a function of distance from the isocenter is investigated by introducing roll and pitch and evaluating the introduced shift for each of the nine targets



**ONE TARGET** at isocenter  
(reference target)

**THREE SPHERES**  
(for image-guided marker fusion)

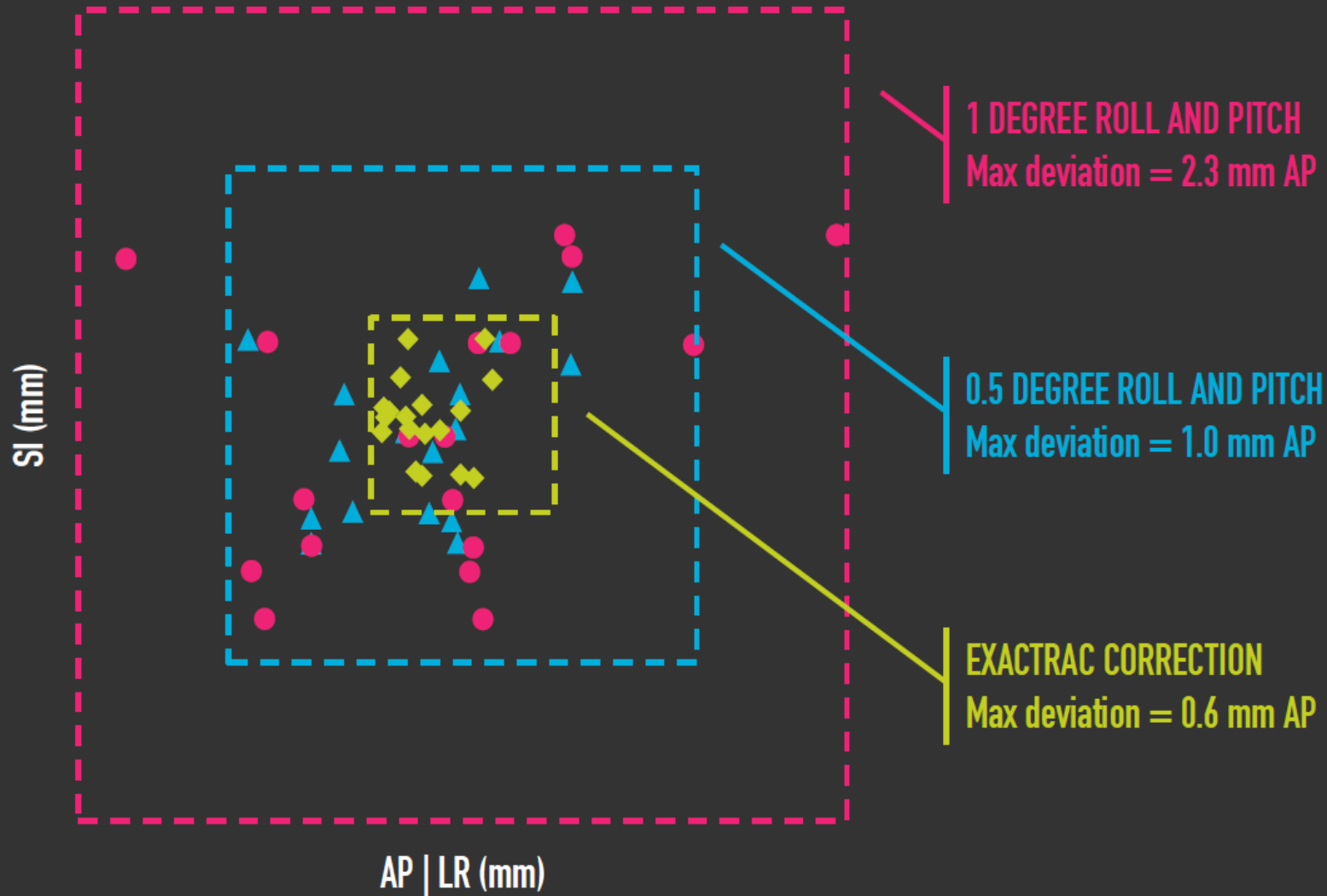
**FOUR TARGETS** at 52 mm  
(covered by 2.5 mm leaves)

**FOUR TARGETS** at 87 mm  
(covered by 5 mm leaves)

A Japanese group build a dedicated phantom with nine spherical metastases to reveal the dramatic effects of uncompensating rotations when treating multiple targets with a single isocenter. They further demonstrate how ExacTrac is able to compensate for these potential errors and realize submillimeter accuracy for all targets



# 3D VECTOR POSITIONING ERRORS FOR EACH TARGET AS A FUNCTION OF ROTATION AND REMAINING ERROR AFTER EXACTRAC CORRECTION



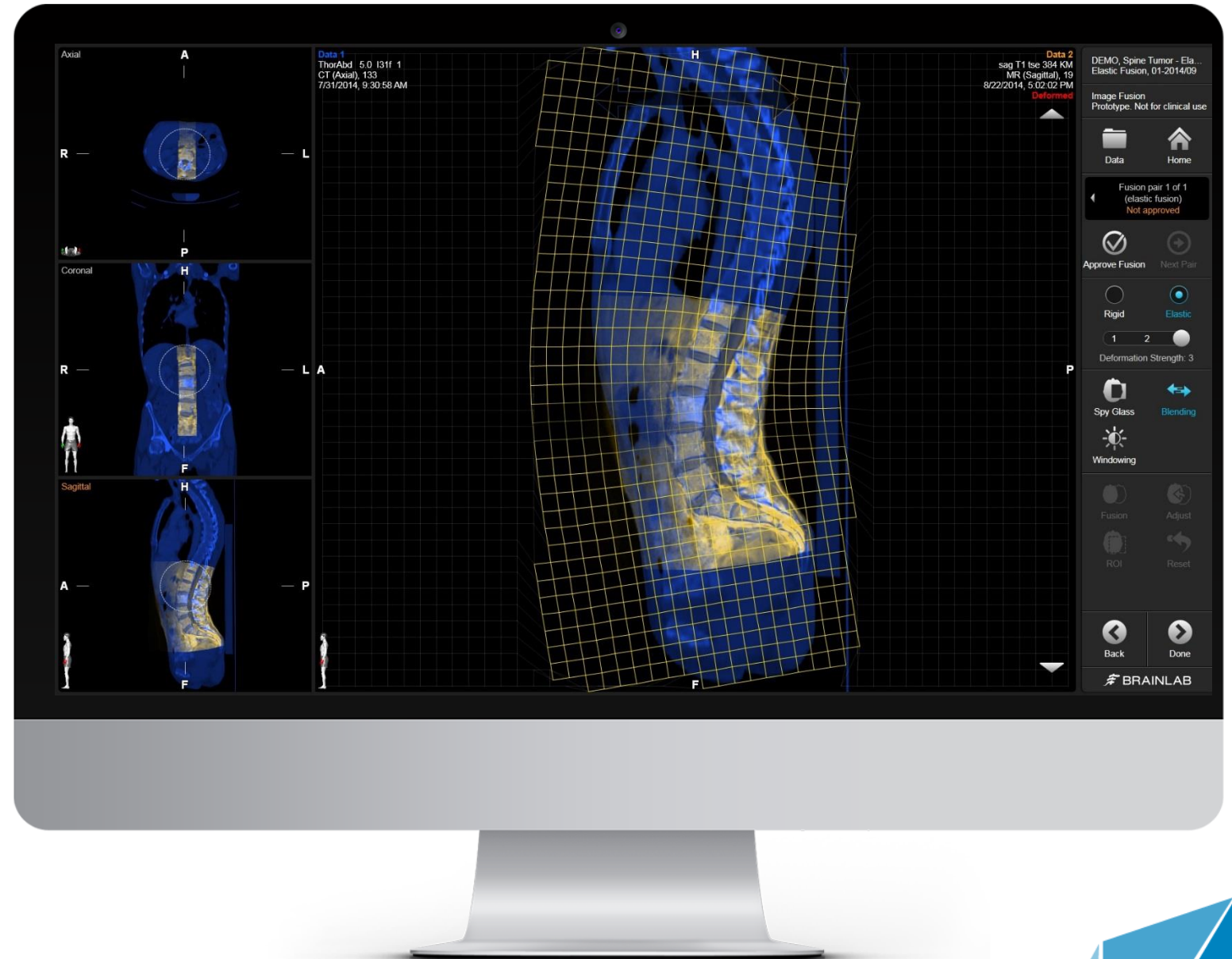
# SPINAL CURVATURE CORRECTION

## IMAGE FUSION con CRANIAL DISTORTION CORRECTION

- Co-registrazione multi-modale deformabile: Cranial MR  $\leftrightarrow$  planning CT
- Permette il contornamento del tumore basato su MR utilizzando il data set corretto con dalla distorsione.
- Nessuna necessita' di operare una fusion locale con ROI

## QUALITY ASSURANCE

- Valutazioni della posizione e grandezza delle distorsioni
- Panoramica rapida su quale MR è la scelta migliore per la definizione precisa del bersaglio
- Facile confronto dei risultati corretti rispetto alla versione rigida o distorta.



# SPINAL CURVATURE CORRECTION

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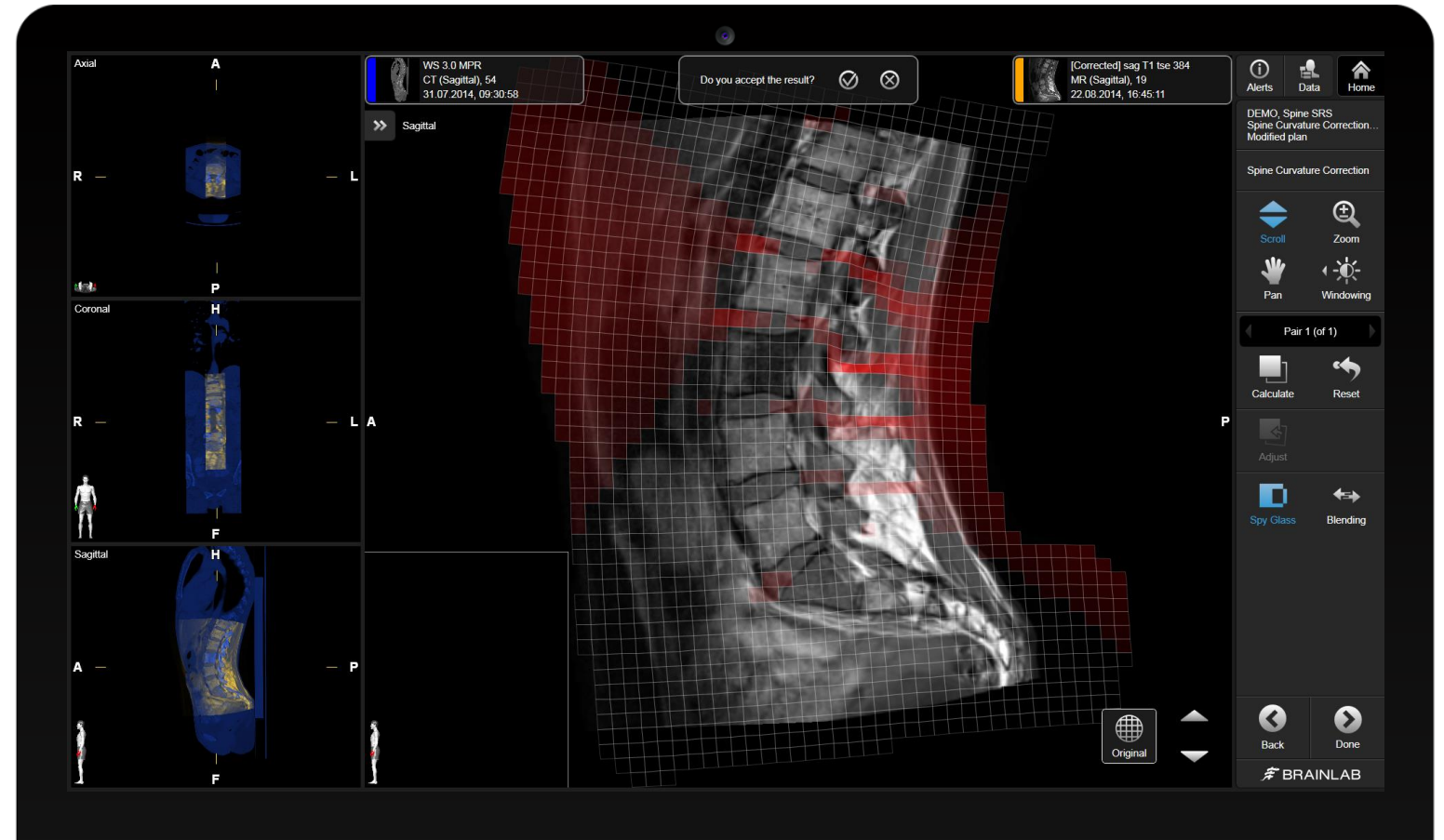
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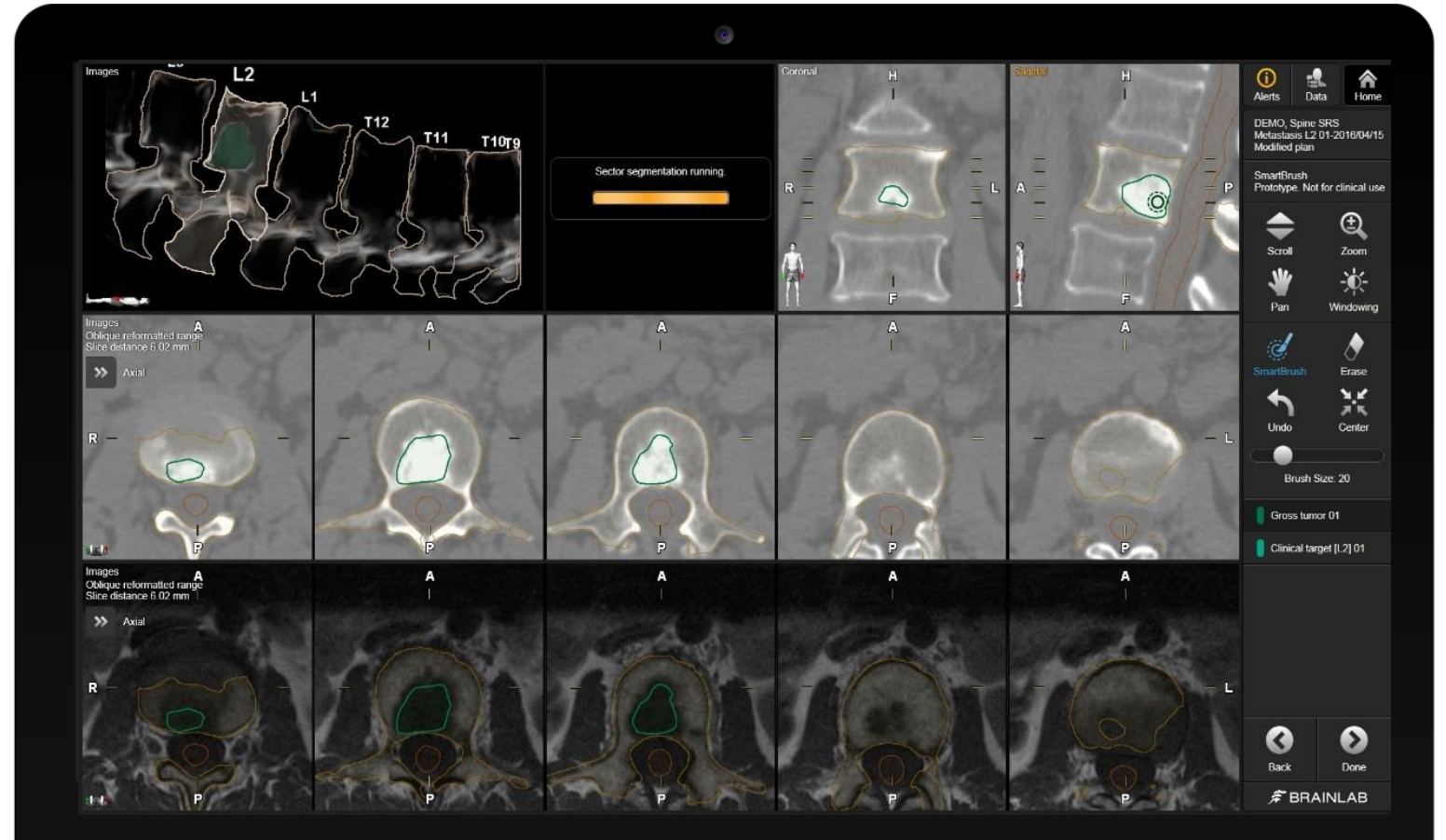
- Valutazioni della posizione e grandezza delle distorsioni
- Panoramica rapida su quale MR è la scelta migliore per la definizione precisa del bersaglio
- Facile confronto dei risultati corretti rispetto alla versione rigida o distorta.



# SPINE SRS ELEMENT

## SPINE SMARTBRUSH

- Funzionalità di contornamento multimodale: due data sets sono utilizzati simultaneamente.
- Segmentazione automatica della vertebra
- Vista specifica per Spine per contornamento con SmartBrush
- Selezione della vertebra di interesse in 3D. Zoom automatico e focalizzato in viste 2D.



# SPINE SRS ELEMENT

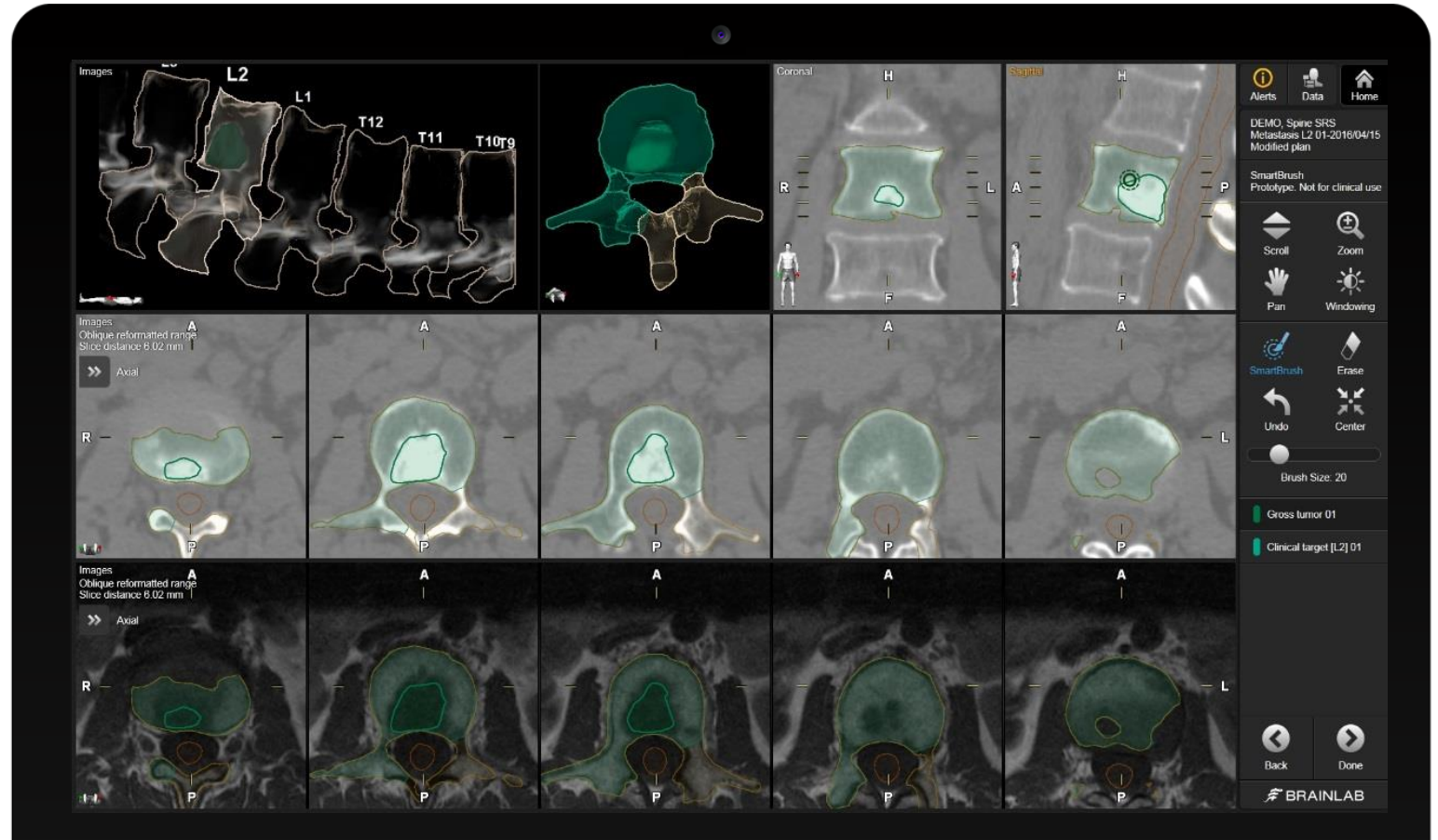
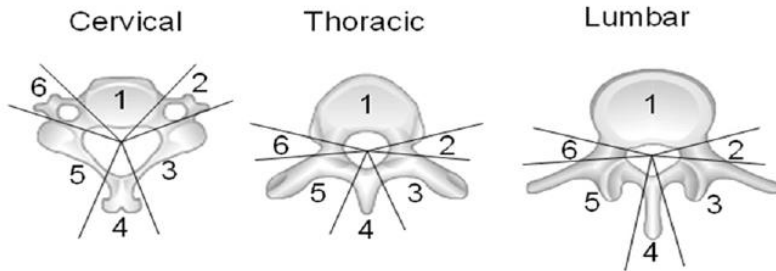


International Journal of  
Radiation Oncology  
biology • physics  
www.redjournal.org

Clinical Investigation: Central Nervous System Tumor

## International Spine Radiosurgery Consortium Consensus Guidelines for Target Volume Definition in Spinal Stereotactic Radiosurgery

Brett W. Cox, MD,<sup>\*1</sup> Daniel E. Spratt, MD,<sup>\*1</sup> Michael Lovelock, PhD,<sup>†</sup>  
Mark H. Bilsky, MD,<sup>‡</sup> Eric Lis, MD,<sup>§</sup> Samuel Ryu, MD,<sup>||</sup> Jason Sheehan, MD,<sup>¶</sup>  
Peter C. Gerszten, MD, MPH,<sup>\*\*</sup> Eric Chang, MD,<sup>††</sup> Iris Gibbs, MD,<sup>‡‡</sup> Scott Soltys, MD,<sup>‡‡</sup>  
Arjun Sahgal, MD,<sup>§§</sup> Joe Deasy, PhD,<sup>†</sup> John Flickinger, MD,<sup>|||</sup> Mubina Quader, PhD,<sup>|||</sup>  
Stefan Mindea, MD,<sup>¶¶</sup> and Yoshiya Yamada, MD,<sup>‡‡</sup>

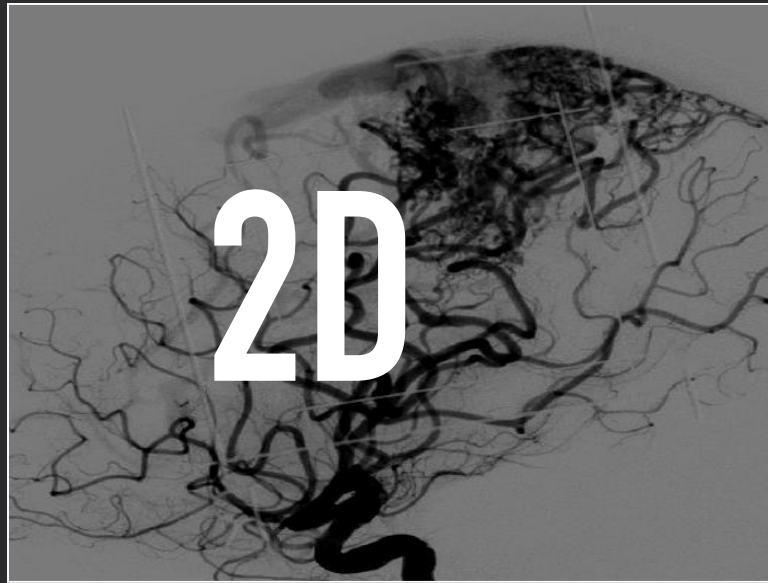


**BRAINLAB ELEMENTS**

# SMARTBRUSH ANGIO



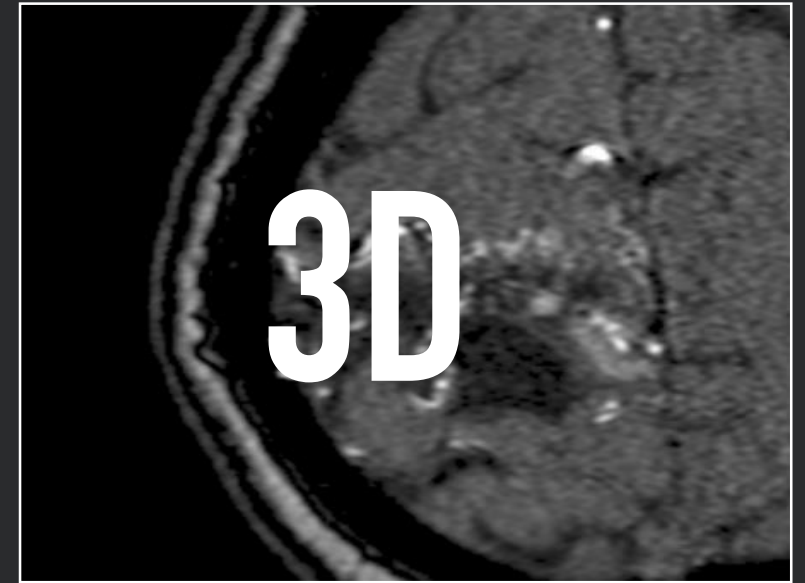
# TRADITIONAL WORKFLOW USING LOCALIZER



MUTUAL  
LOCALIZATION



INVASIVE HEAD FRAME  
REPEATED  
ANGIOGRAPHY





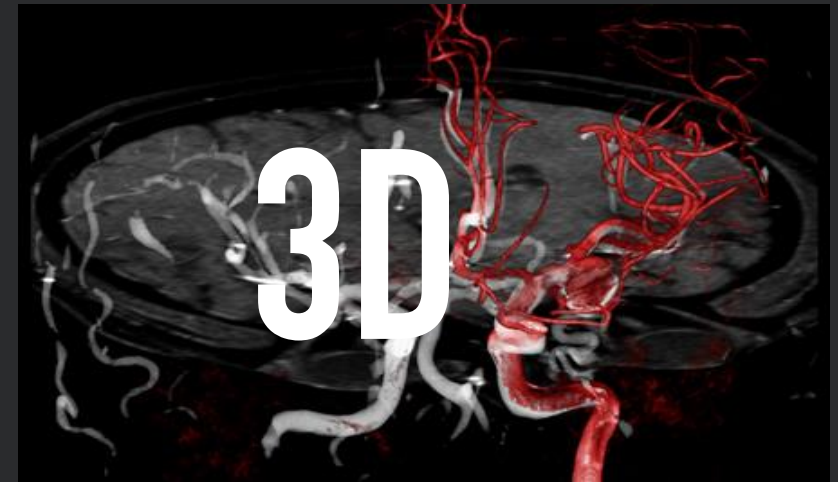
# SMARTBRUSH ANGIO WORKFLOW



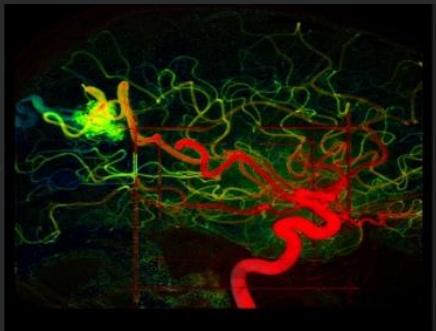
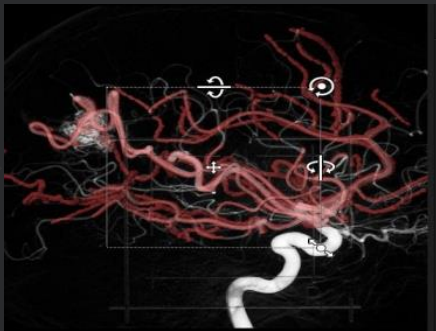
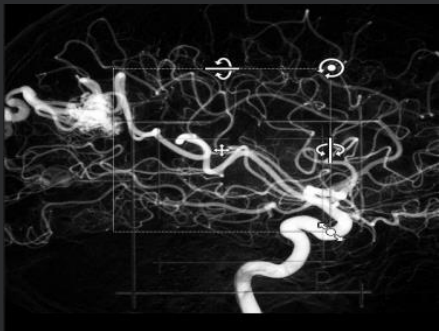
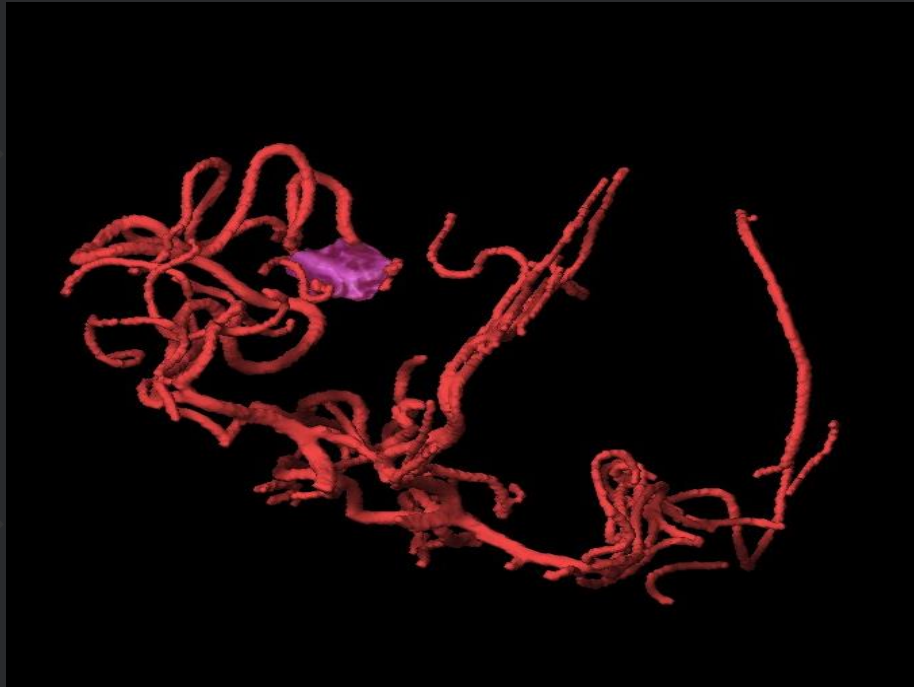
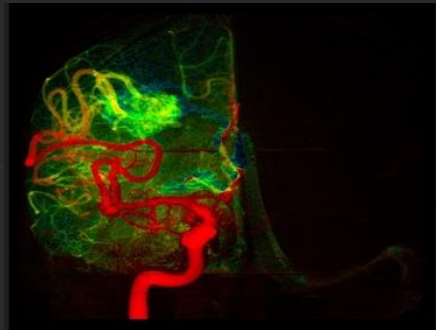
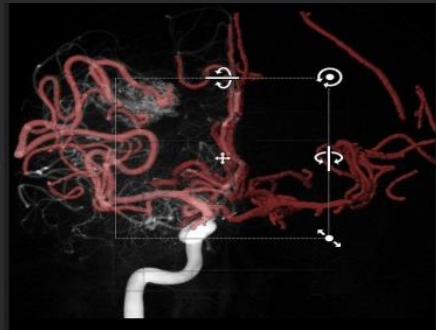
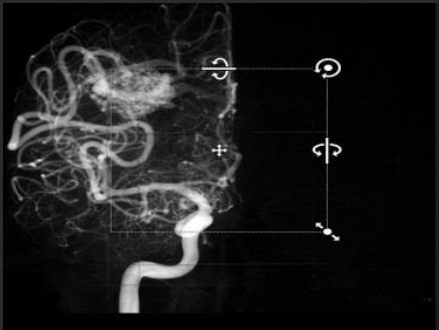
VESSEL TREE  
FUSION



FRAMELESS MASK  
NO ADDITIONAL  
ANGIOGRAPHY



# SMARTBRUSH ANGIO WORKFLOW



**1**

2D TO 3D  
VESSEL  
TREE FUSION

**2**

COLOR  
INTENSITY  
PROJECTION  
ROI

**3**

AUTOMATIC  
NIDUS  
SEGMENTATION

# 2D TO 3D VESSEL TREE FUSION

Frontal  
Time Frame 12 of 33

Stereotaxie

Lateral Left  
Time Frame 13 of 38

Stereotaxie

DEMO, RT Angio Planning  
Cranial AVM, MR XA

Angio Planning  
Prototype. Not for clinical use

Data Home

Fusion Undo Fusion

Vessel Visible

Vessel Complexity

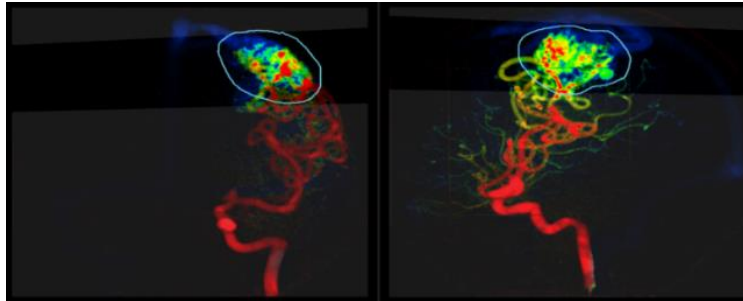
Data Fusion ROI Brush

Back Next

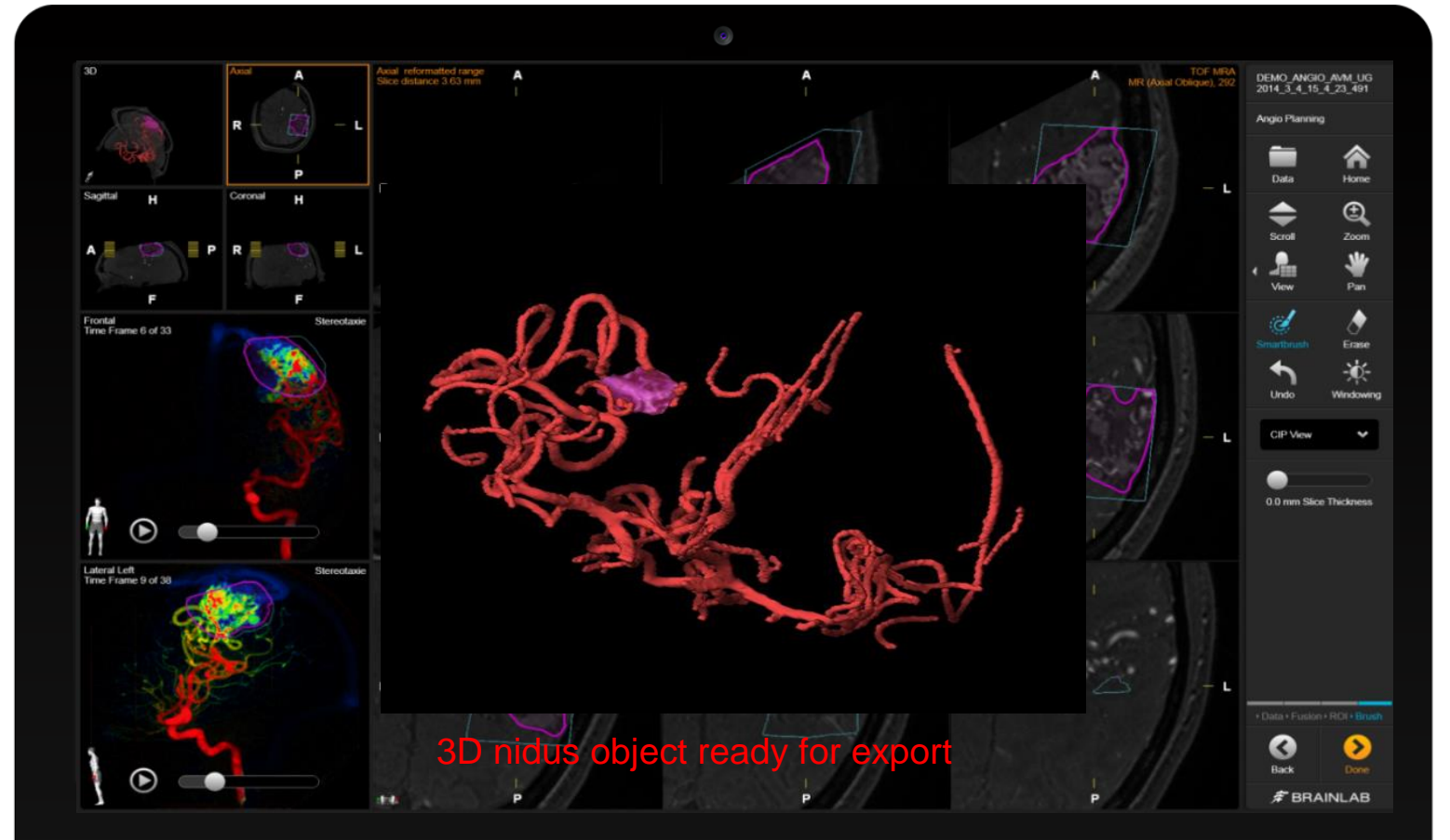
BRAINLAB

# ROI OUTLINING

Color Intensity Projection (CIP) view



# NIDUS GENERATION



**BRAINLAB ELEMENTS**

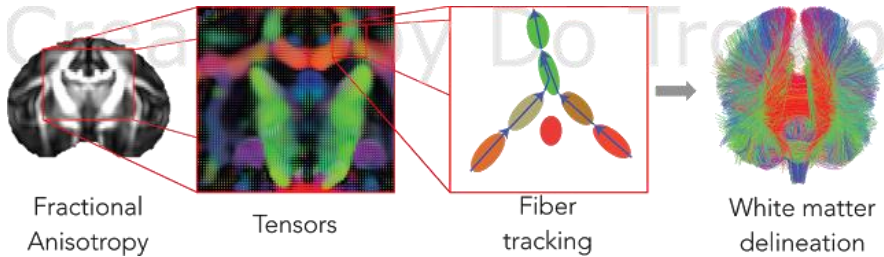
**FIBERTRACKING**



# FIBERTRACKING

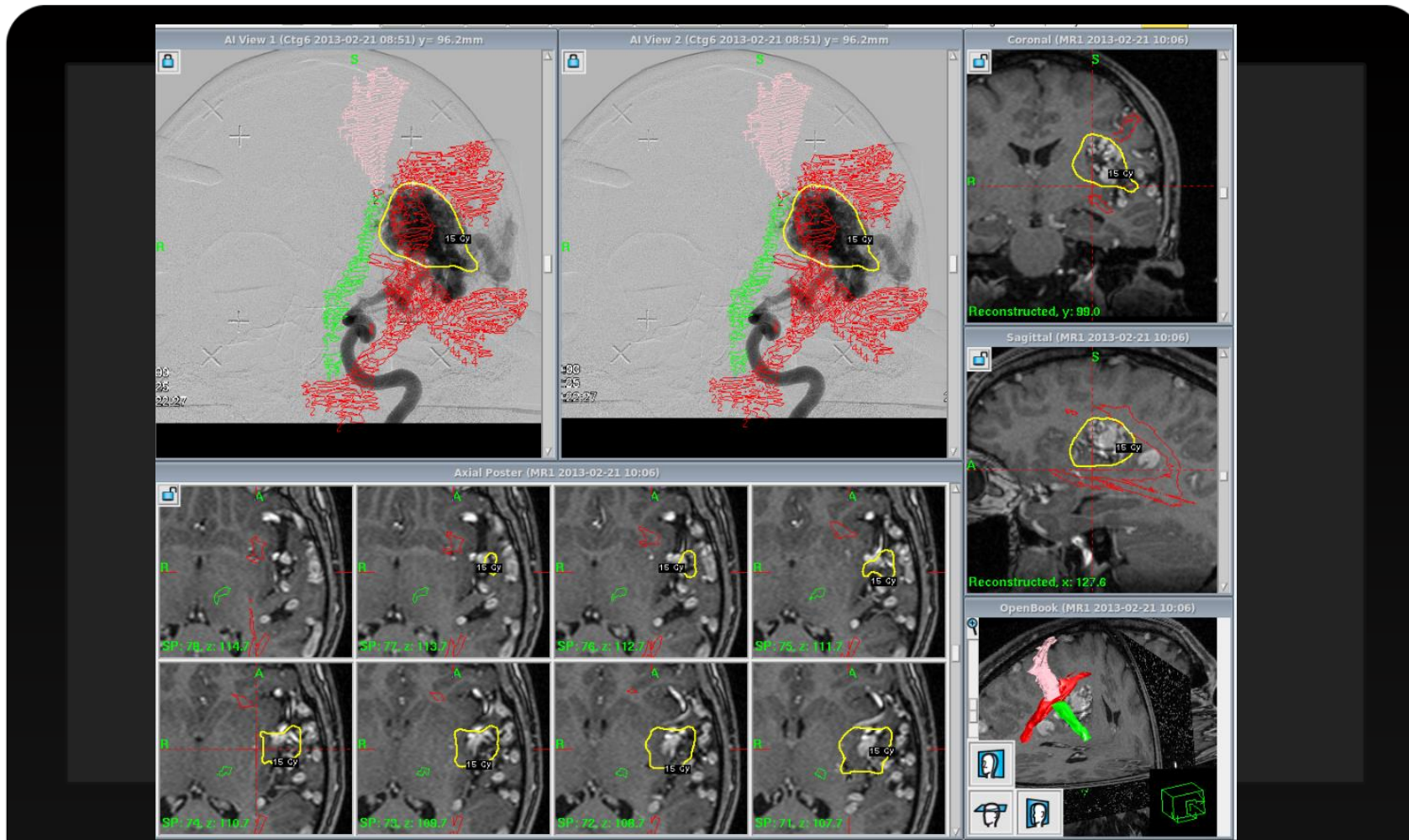
## FUNCTIONAL PLANNING ELEMENT

- Completamente automatizzato e DTI Data Preprocessing migliorato: Motion- / Eddy Current Correction, Denoising, Riallineamento B-Vector.
- Supporto di Fusione Elastica
- Accesso veloce & intuitivo all'atlas-based inclusione/esclusione del Tracking delle ROI
- Vista Brain Projection per una pianificazione funzionale intuitiva e revisione
- Fibertracking "On-the-Fly"

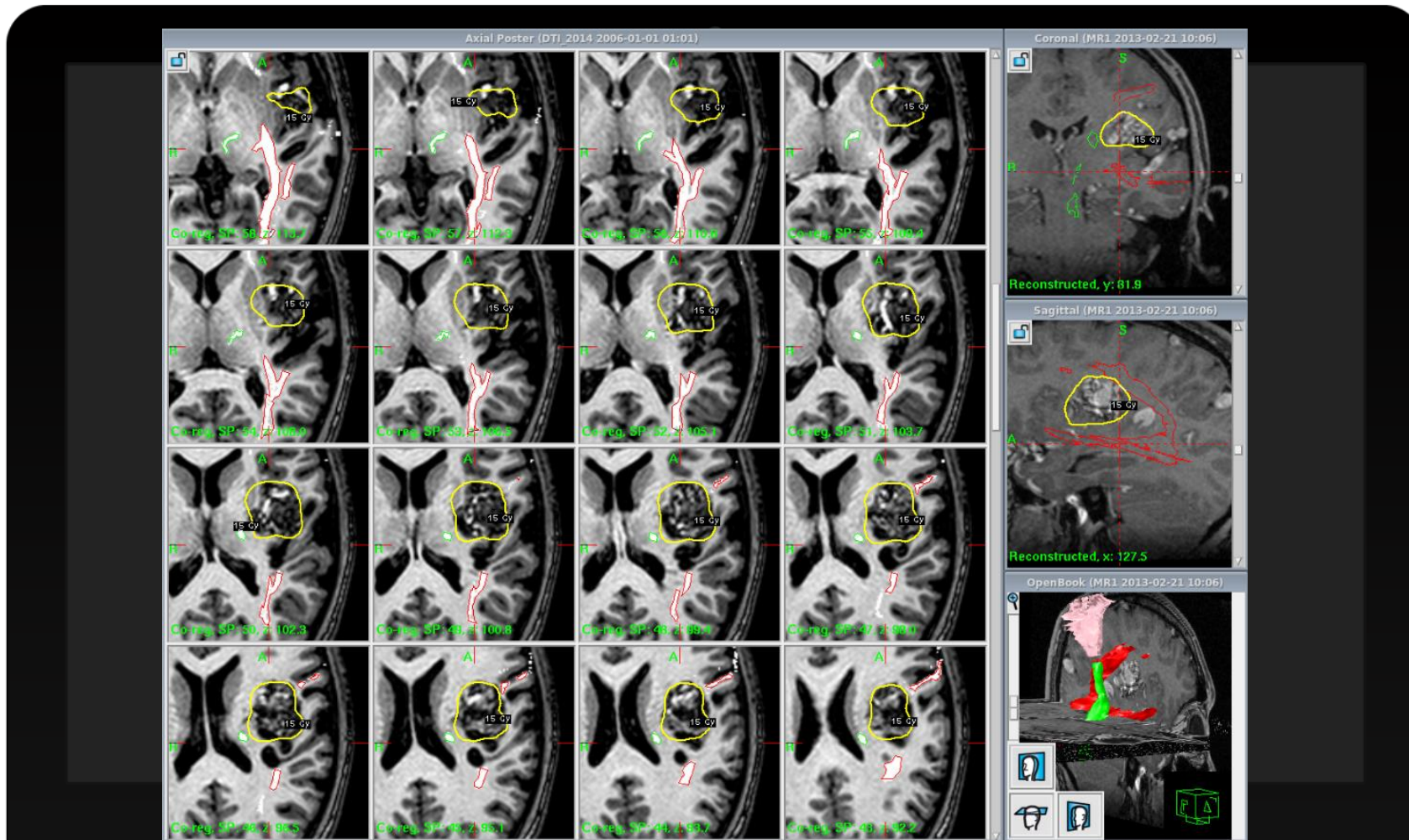








Courtesy of  AZIENDA OSPEDALIERA UNIVERSITARIA INTEGRATA VERONA 

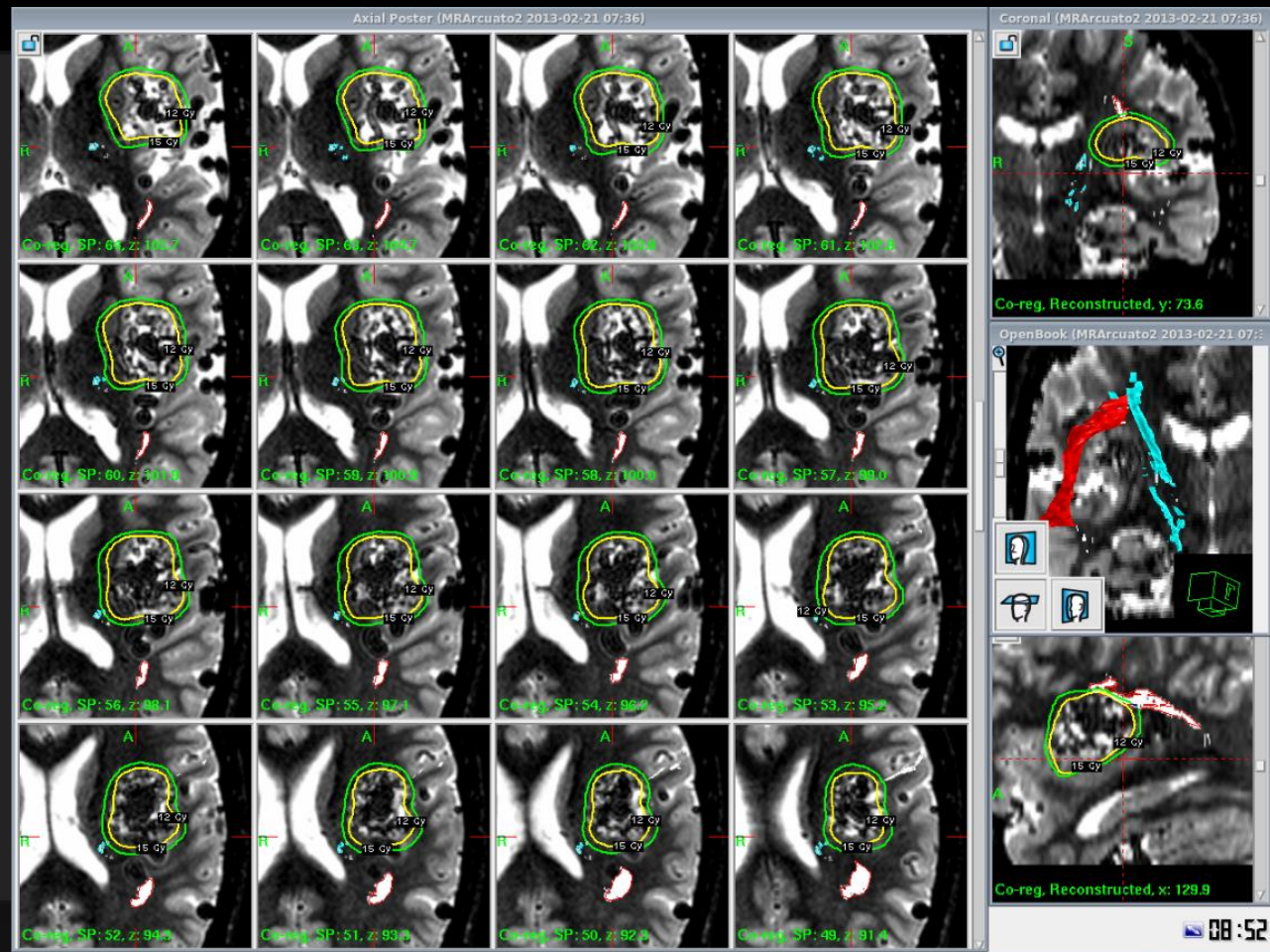


Courtesy of



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VERONA





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# Photon and proton therapy planning comparison for malignant glioma based on CT, FDG-PET, DTI-MRI and fiber tracking

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• Pages 777-783 | Received 16 Mar 2011, Accepted 13 Apr 2011, Published online: 18 Jul 2011

## Abstract

**Purpose.** The purpose of this study was to compare treatment plans generated using fixed beam Intensity Modulated photon Radiation Therapy (IMRT), inversely optimized arc therapy (RapidArc(R), RA) with spot-scanned Intensity Modulated Proton Therapy (IMPT) for high-grade glioma patients. Plans were compared with respect to target coverage and sparing of organs at risk (OARs), with special attention to the possibility of hippocampus sparing.

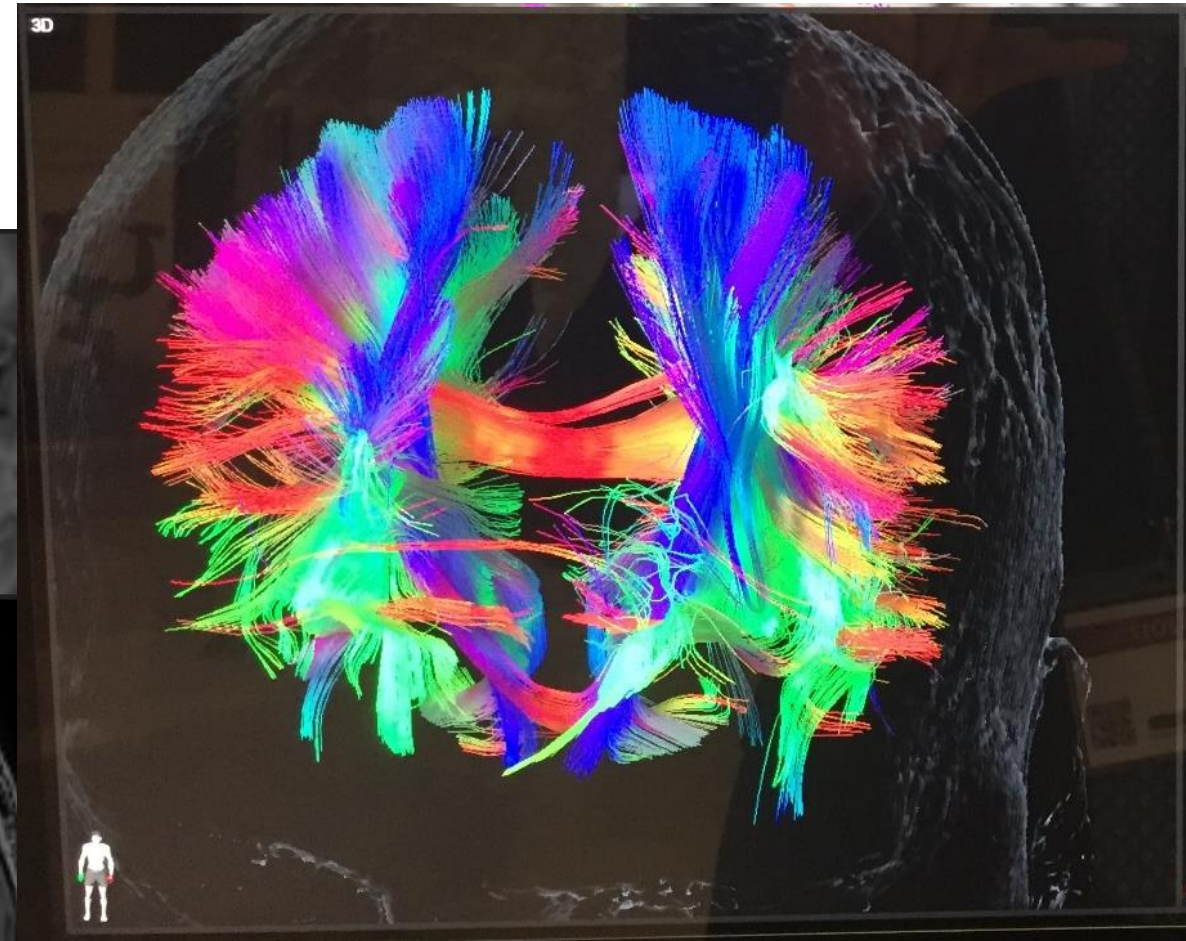
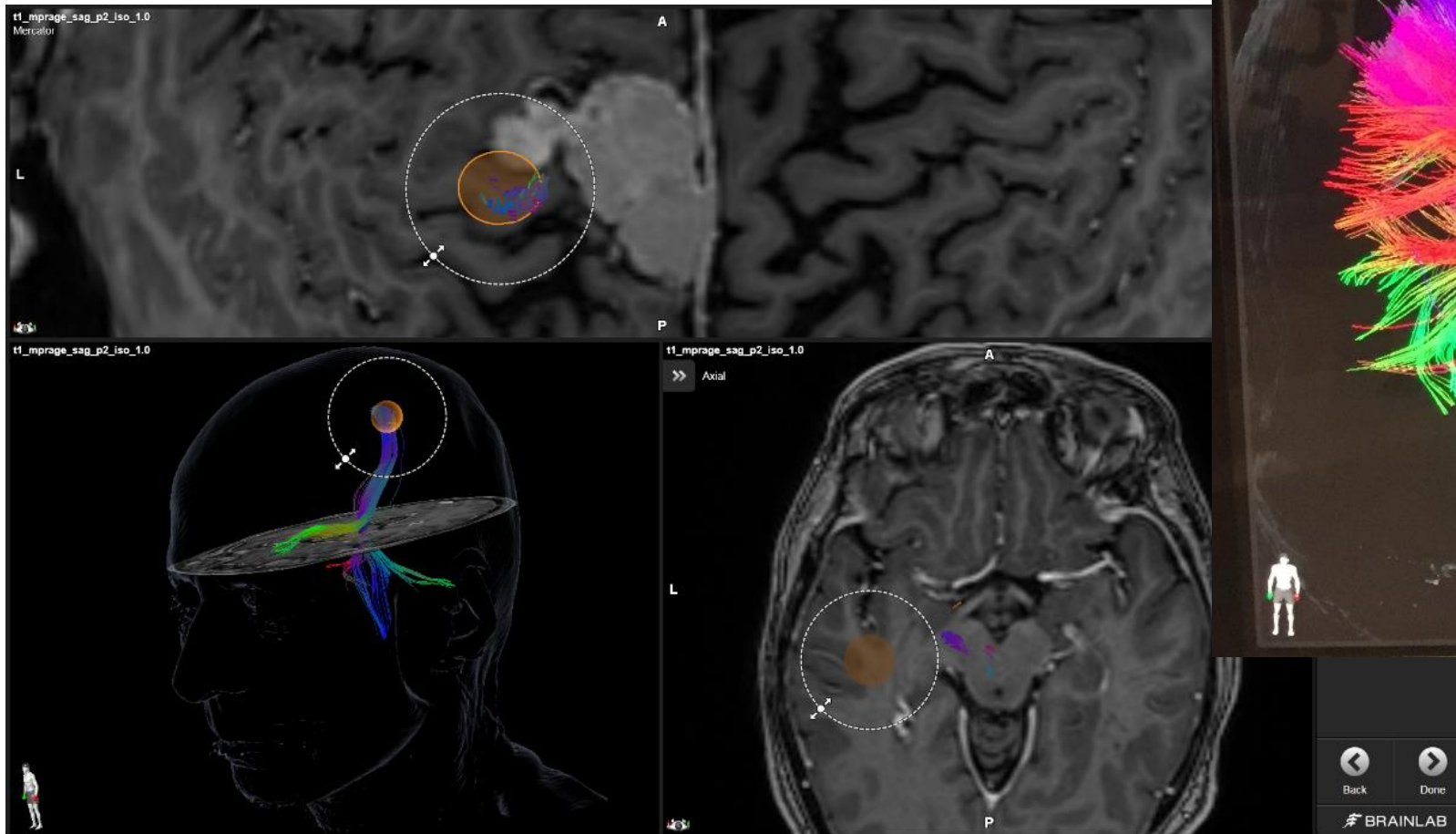
**Method.** Fifteen consecutive patients diagnosed with grade III and IV glioma were selected for this study. The target and OARs were delineated based on computed tomography (CT), FDG-positron emission tomography (PET) and T1-, T2-weighted, and Diffusion Tensor Imaging (DTI) magnetic resonance imaging (MRI) and fiber-tracking. In this study, a 6 MV photon beam on a linear accelerator with a multileaf collimator (MLC) with 2.5 mm leaves and a spot-scanning proton therapy machine were used. Two RA fields, using both a coplanar (clinical standard) and a non-coplanar, setup was compared to the IMRT and IMPT techniques. Three and three to four non-coplanar fields were used in the spot-scanned IMPT and IMRT plans, respectively. The same set of planning dose-volume optimizer objective values were used for the four techniques. The highest planning priority was given to the brainstem (maximum 54 Gy) followed by the PTV (prescription 60 Gy); the hippocampi, eyes, inner ears, brain and chiasm were given lower priority. Doses were recorded for the plans to targets and OARs and compared to our clinical standard technique using the Wilcoxon signed rank test.

**Result.** The PTV coverage was significantly more conform for IMPT than the coplanar RA technique, while RA plans tended to be more conform than the IMRT plans, as measured by the standard deviation of the PTV dose. In the cases where the tumor was confined in one cerebral hemisphere (eight patients), the non-coplanar RA and IMPT techniques yielded borderline significantly lower doses to the contralateral hippocampus compared to the standard (22% and 97% average reduction for non-coplanar RA and IMPT, respectively). The IMPT technique allowed for the largest healthy tissue sparing of the techniques in terms of whole brain doses and to the fiber tracts. The maximum doses to the chiasm and brainstem were comparable for all techniques.

**Conclusion.** The IMPT technique produced the most conform plans. For tumors located in the one of the cerebral hemispheres, the non-coplanar RA and the IMPT techniques were able to reduce doses to the contralateral hippocampus. The IMPT technique offered the largest sparing of the brain and fiber tracts. RA techniques tended to produce more conform target doses than IMRT.

# FIBERTRACKING

"Diffusion Tensor Imaging is a cutting edge imaging technique that provides quantitative information with which to visualize and study connectivity and continuity of neural pathways in the central and peripheral nervous systems *in vivo*." (Basser et al. 2000).



# BRAINLAB ELEMENTS

*4II* ALGORITHM

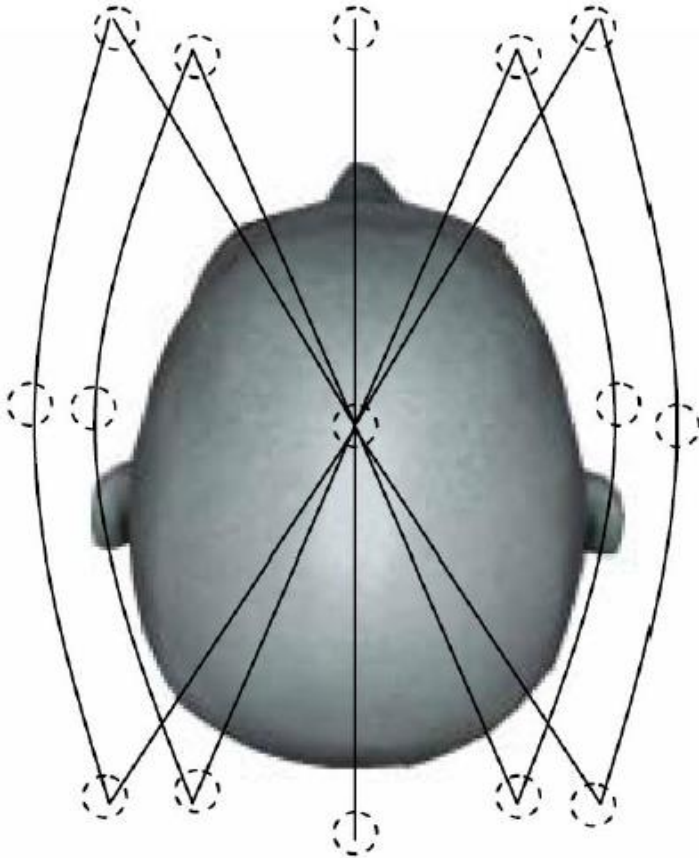
# **TRAJECTORY- BASED TREATMENT PLANNING AND DELIVERY FOR CRANIAL RADIOSURGERY**

**JAMES ROBAR, PHD, FCCPM**

**LEE MACDONALD, MSC**

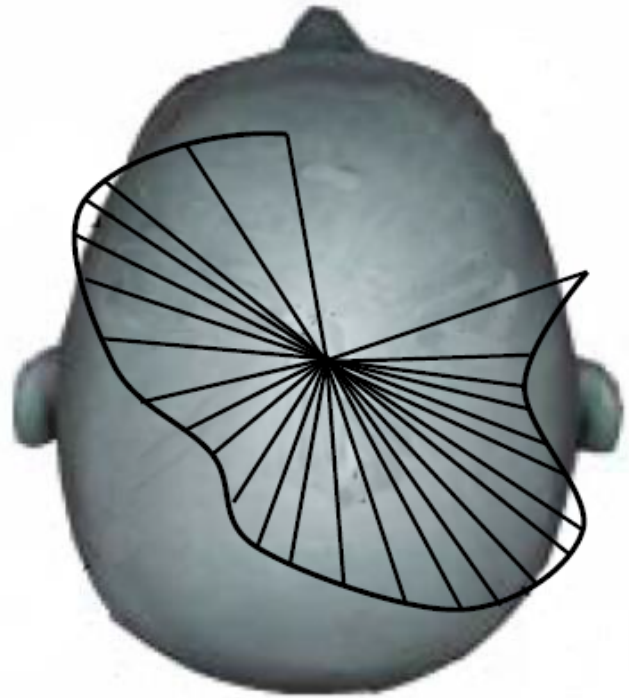
**CHRISTOPHER THOMAS, PHD, MCCPM**

**DALHOUSIE UNIVERSITY, CANADA**



- Identical arc arrangement at cardinal angles for all cases
- No patient-specific customization to the arc arrangement
- Cranial cases are highly variable with regard to PTV and OAR geometry

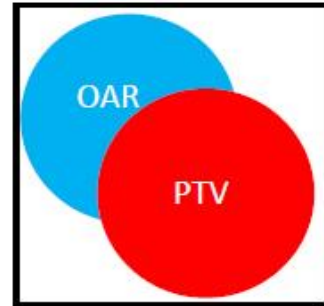




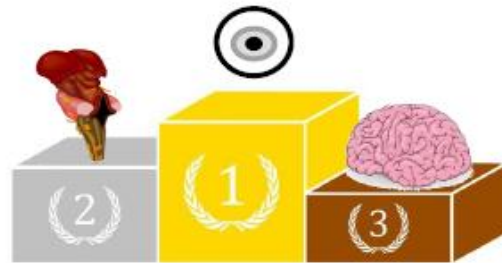
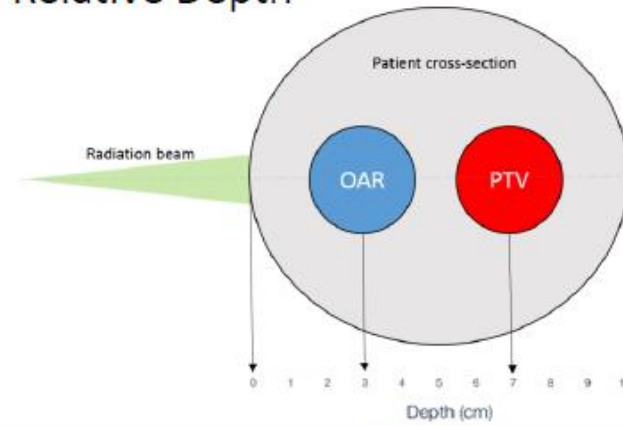
- Establish patient-tailored dynamic arc trajectories
- May involve coordinated gantry and couch motion
- Designed to minimize dose to OARs without compromising PTV coverage

## Algorithm Objectives

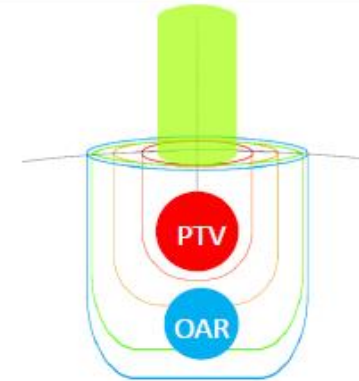
Overlap between PTV and OAR



Relative Depth



QUANTEC Dose Weighting

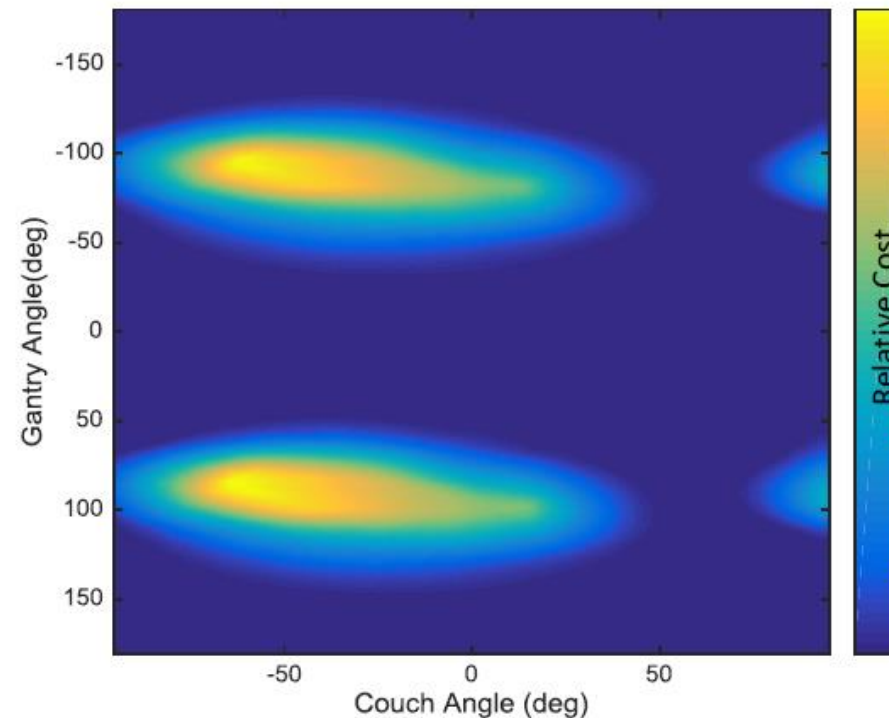


Promote Rapid Dose Fall-off

# OAR OVERLAP in FOUR-PI

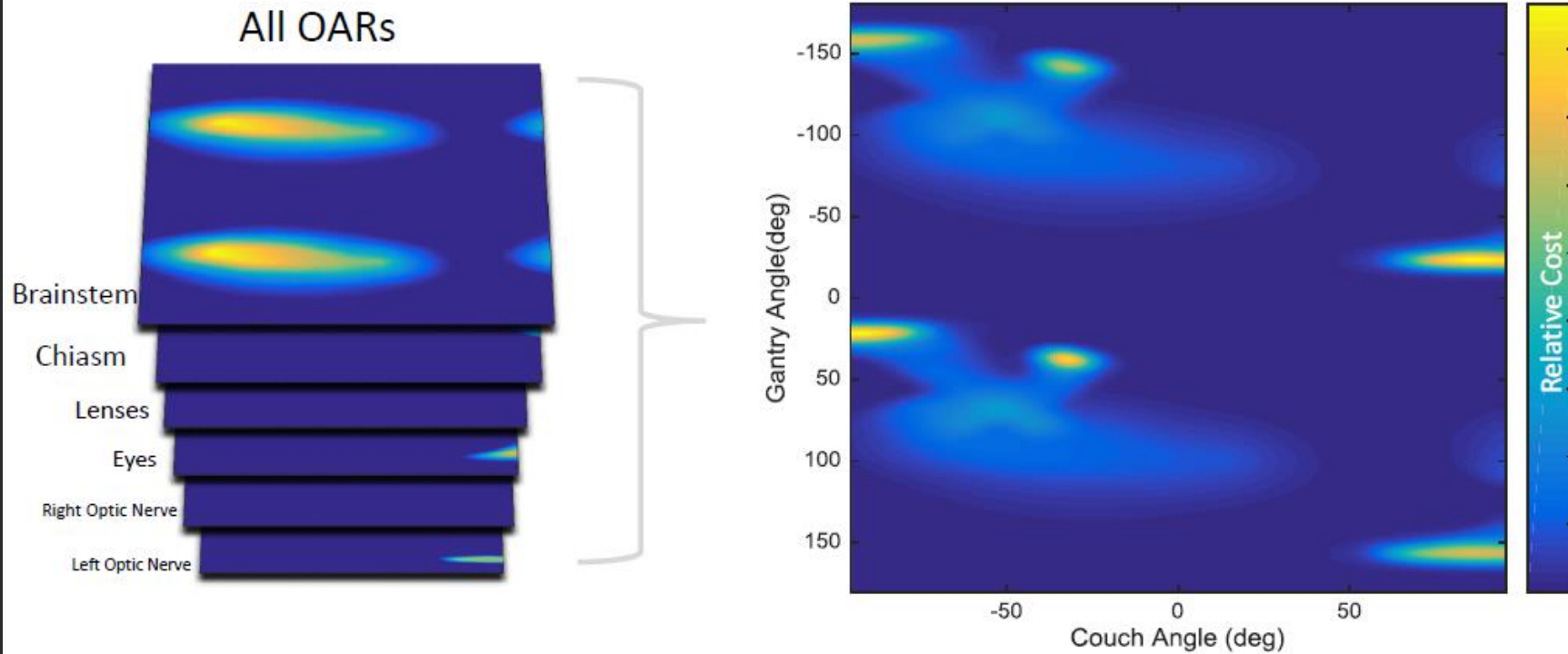
- Creates a suitability ranking for every couch-gantry position
- Unique map for every patient
- Condenses three dimensional relationships between structures
- Higher penalty assigned with OAR in front of PTV

## EXAMPLE: brainstem map



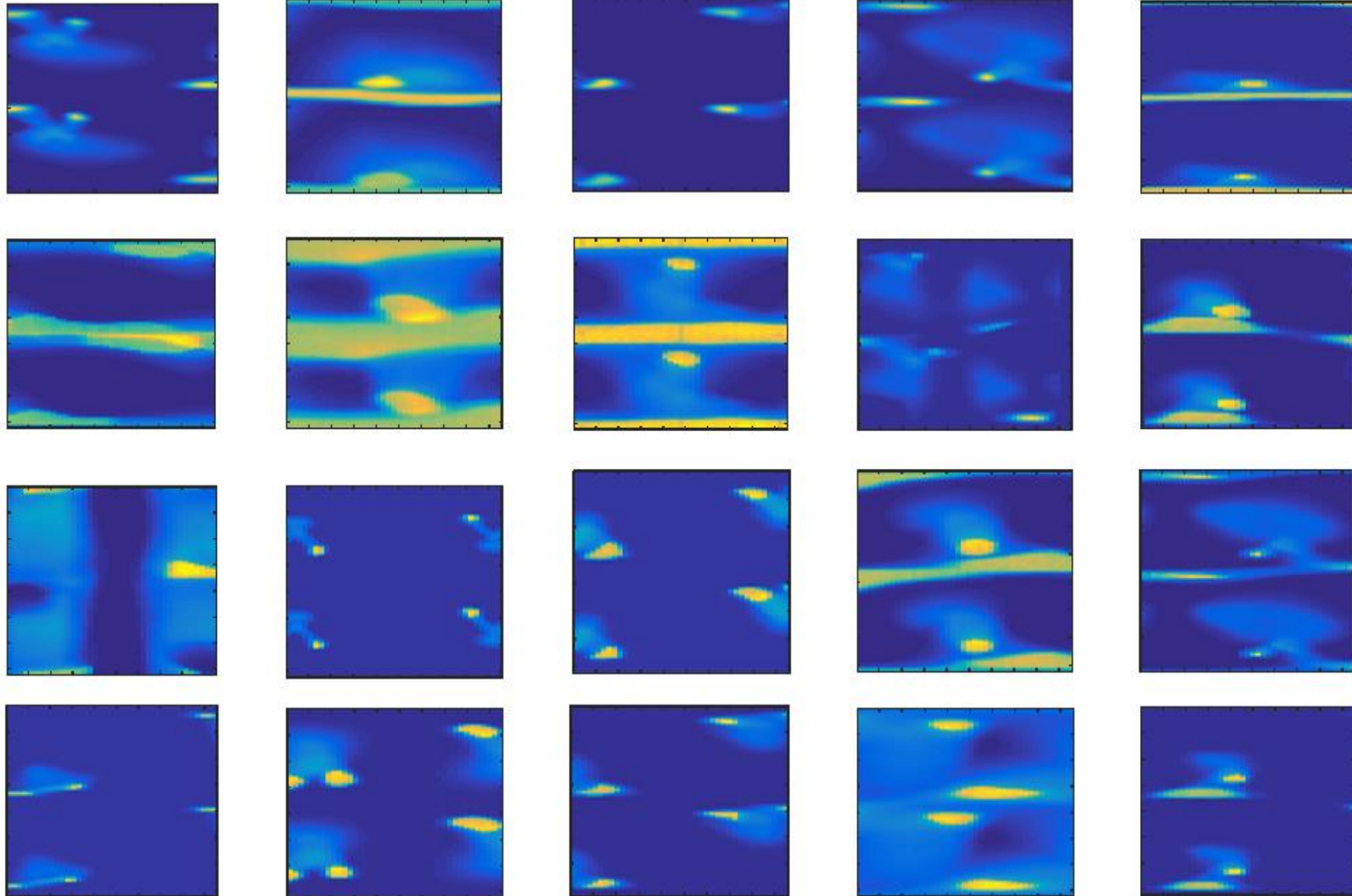
# OAR OVERLAP in FOUR-PI

## A composite OAR map



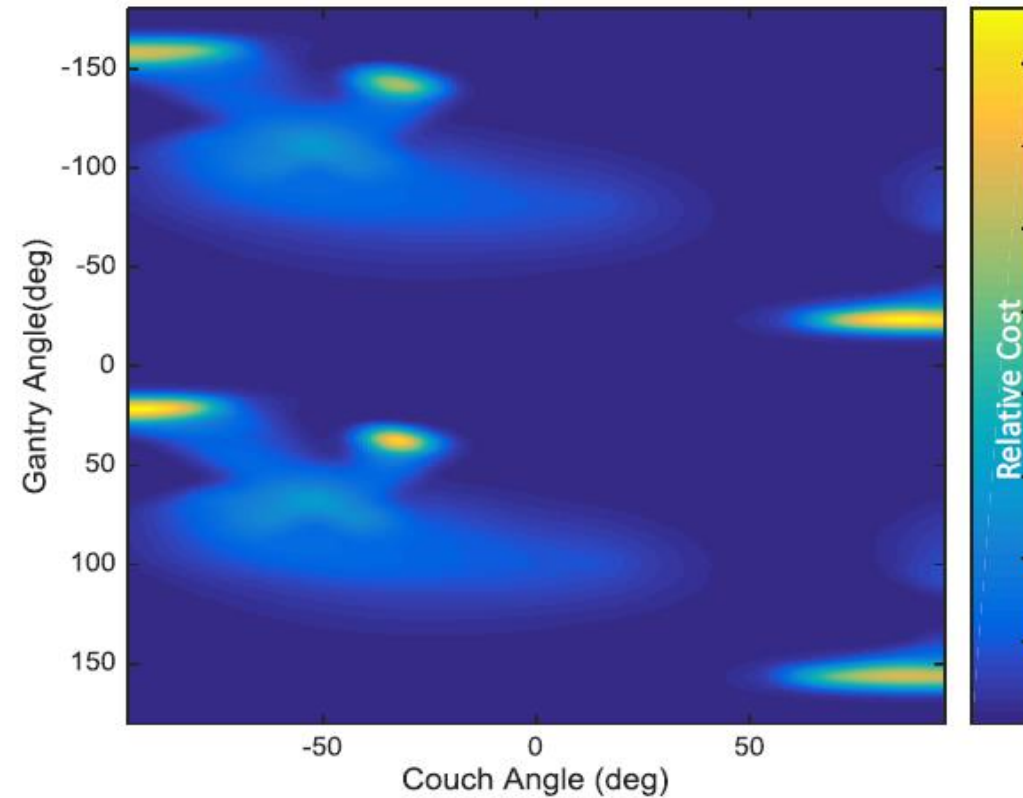
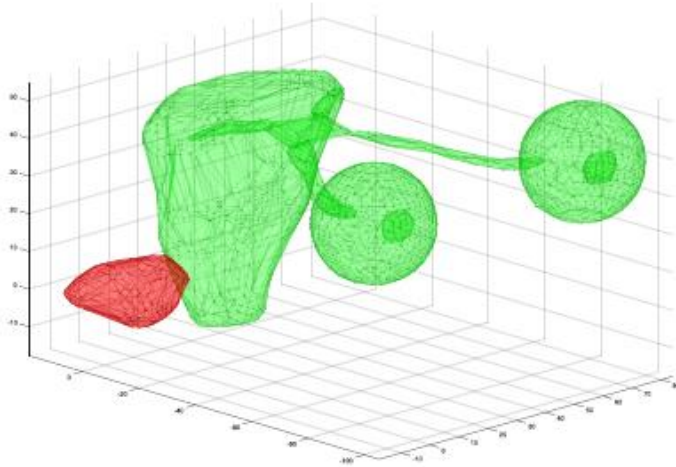
# SAMPLE OVERLAP MAPS

20 CRANIAL RADIO SURGERY PATIENTS



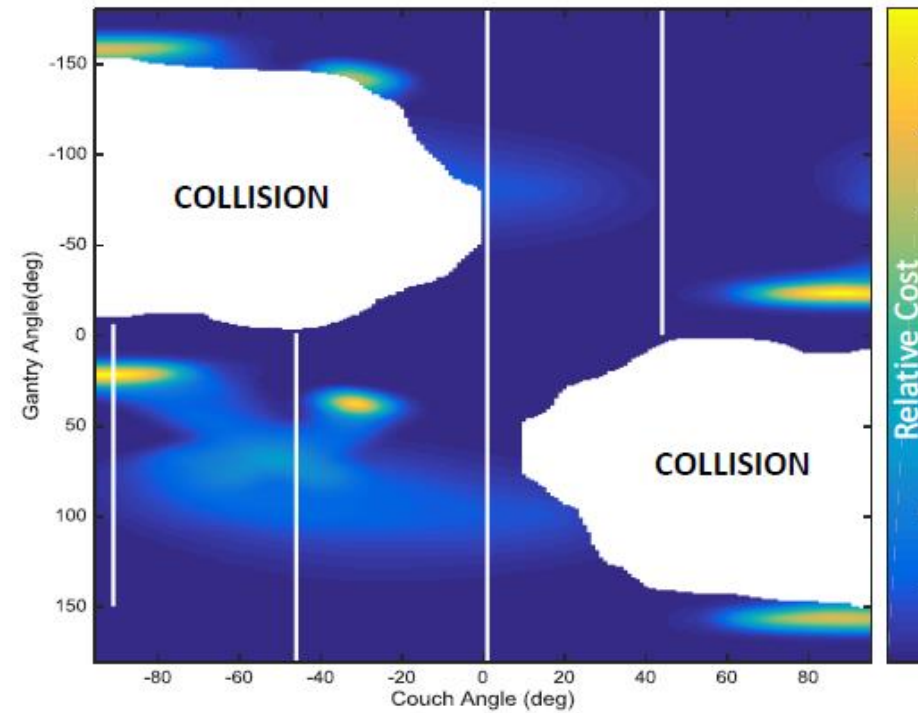
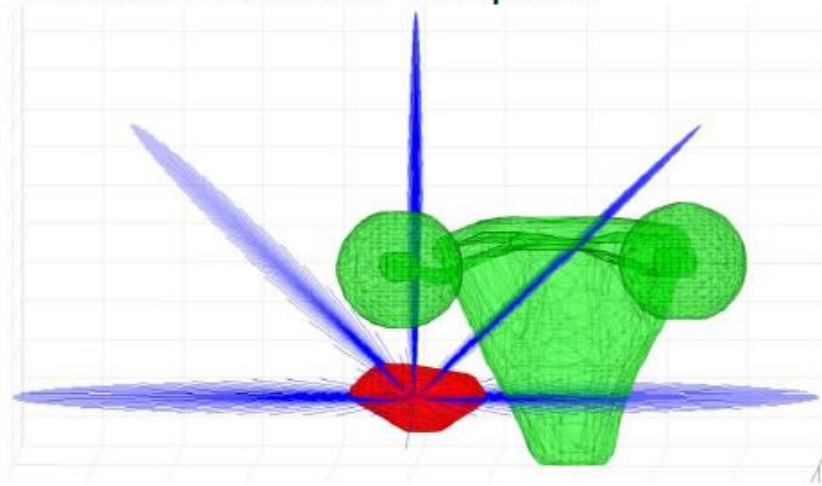
## Patient Example

- Right Acoustic Neuroma.
  - Brainstem
  - Eyes
  - Lenses
  - Optic Chiasm
  - Optic Nerves

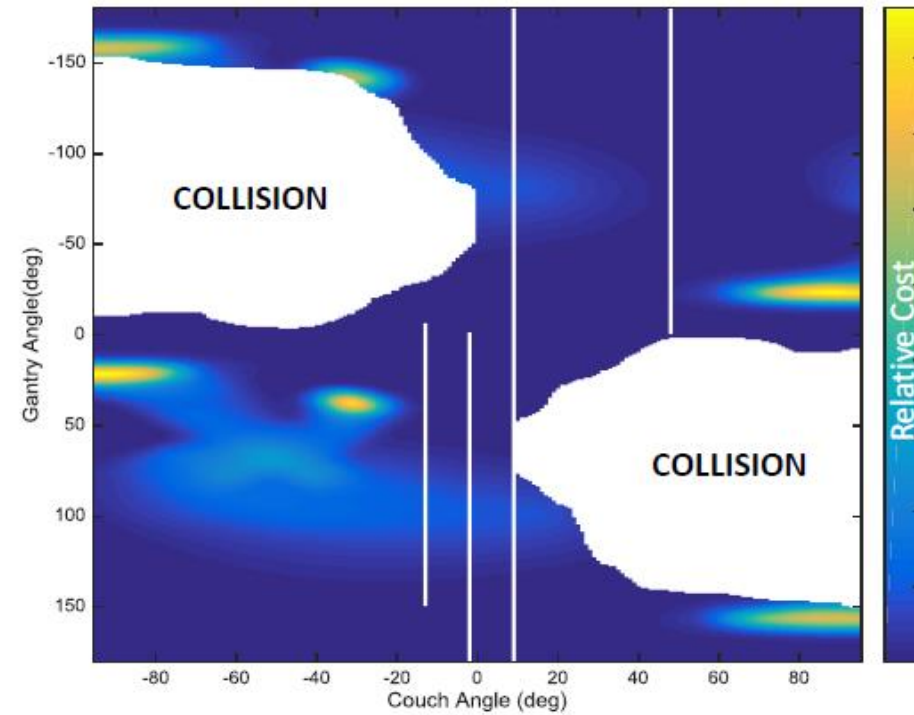
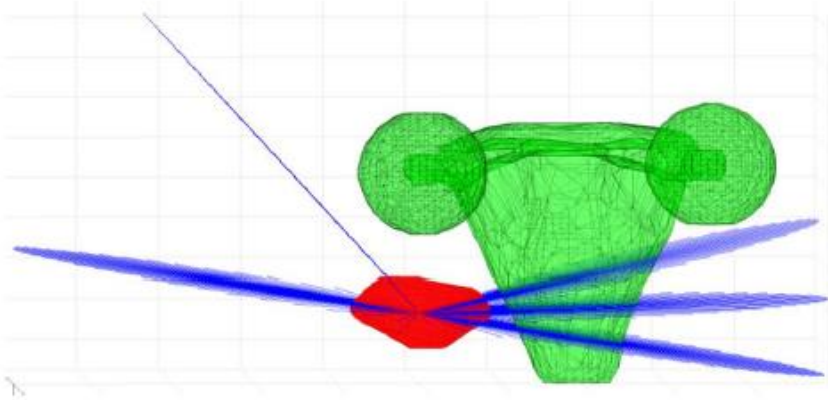


## Conventional Class Solution

Standard cranial template

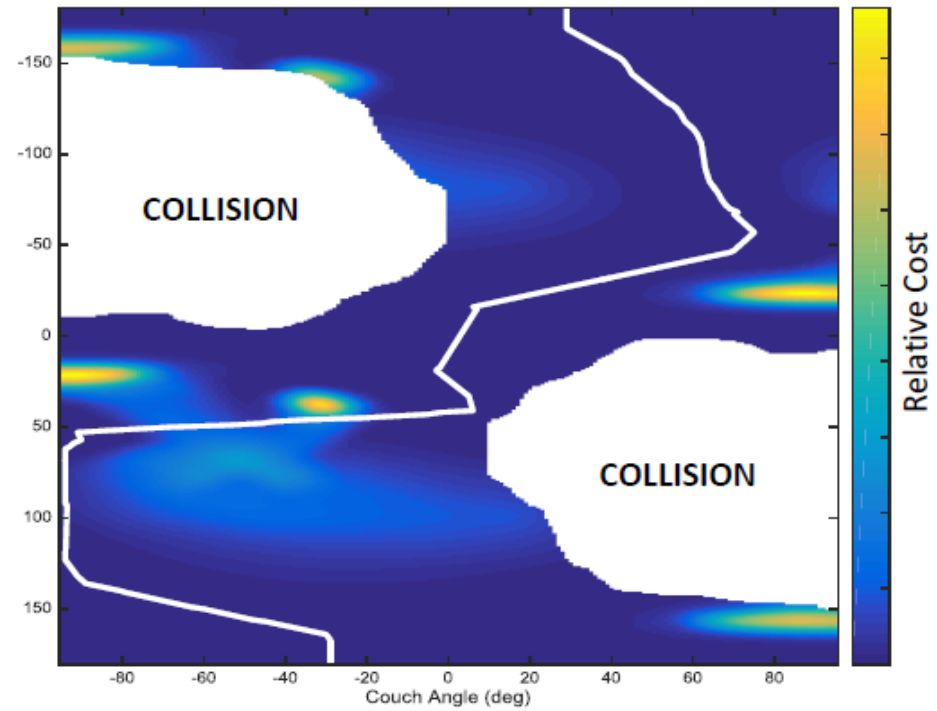
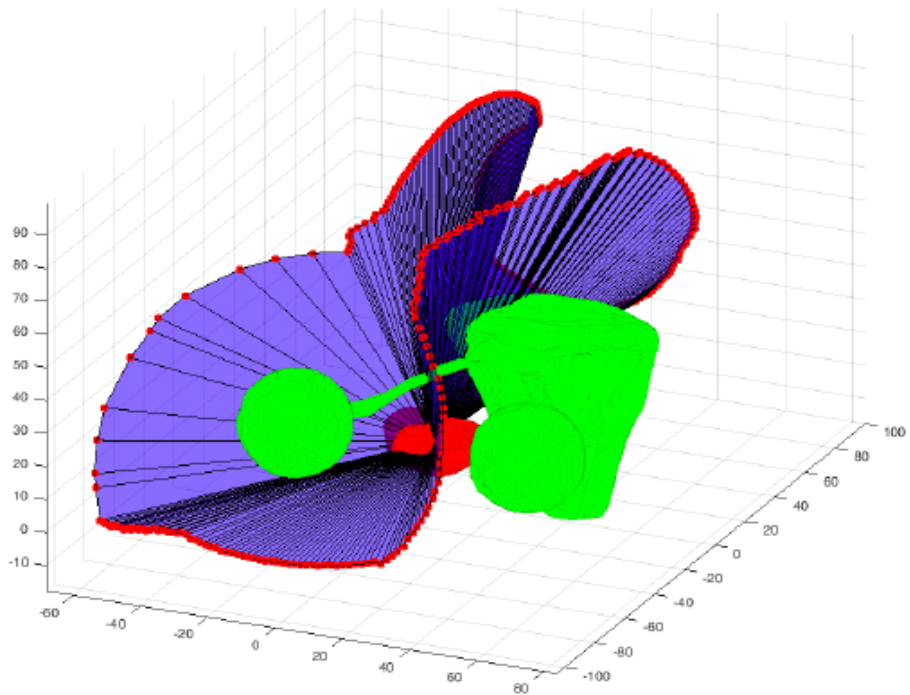


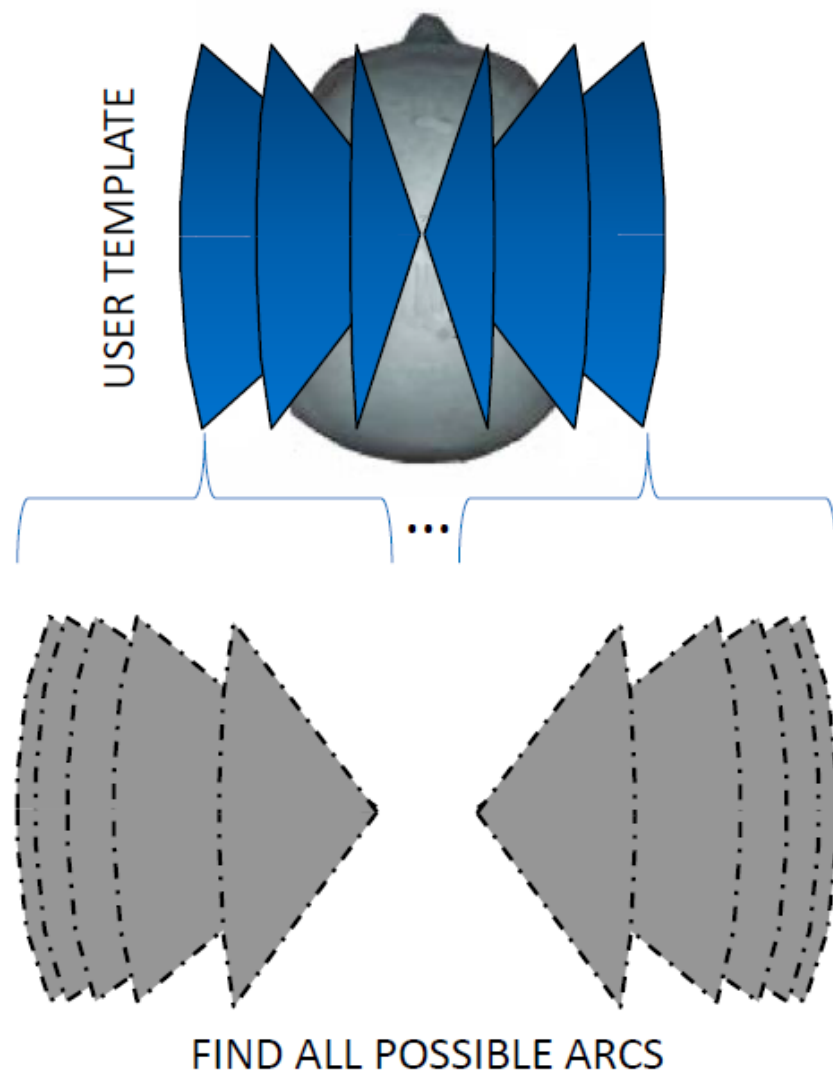
## Fixed-Couch Optimization





# DYNAMIC TRAJECTORY





**Arc Setup Optimization**

- Arc Setup Optimization is enabled: Yes
- Minimum table angle distance between arcs: 20.000000
- Minimum distance to 90°/270° table angle: 0.000000
- Importance of deviation of table angles: 0.500000
- Importance of deviation of gantry angles: 0.200000
- Importance of OAR-PTV overlap: 1.000000
- Importance of PTV radiological depth: 0.500000
- Minimum span per arc: 90.000000

↑ FIND BEST POSSIBLE SET



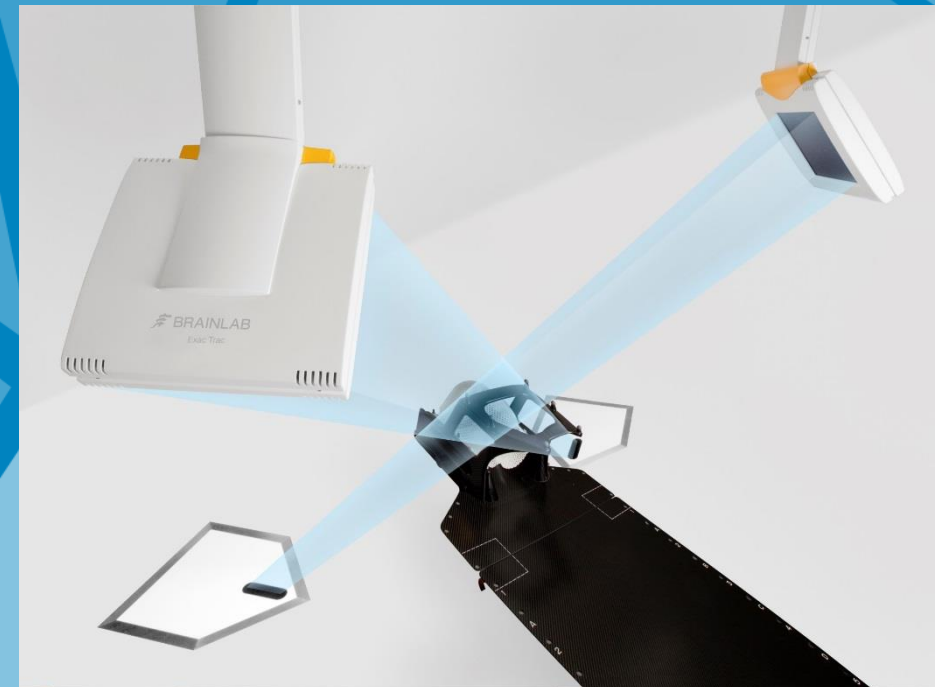
- PTV/OAR overlap
- OAR radiological depth
- OAR on source side
- Gantry stop/start deviations
- Table deviations

ASSIGN PENALTIES



# EXACTRAC X-RAY

PRECISIONE

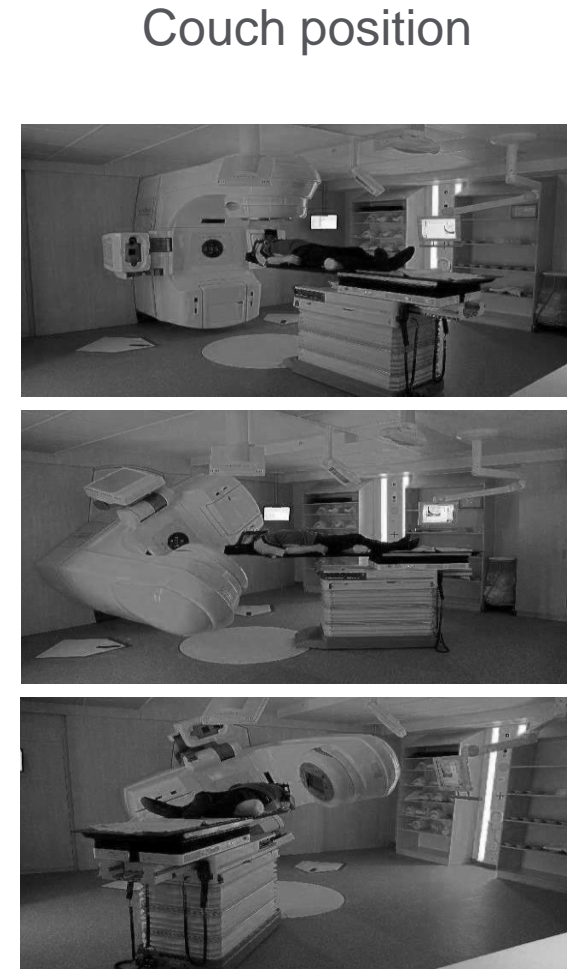
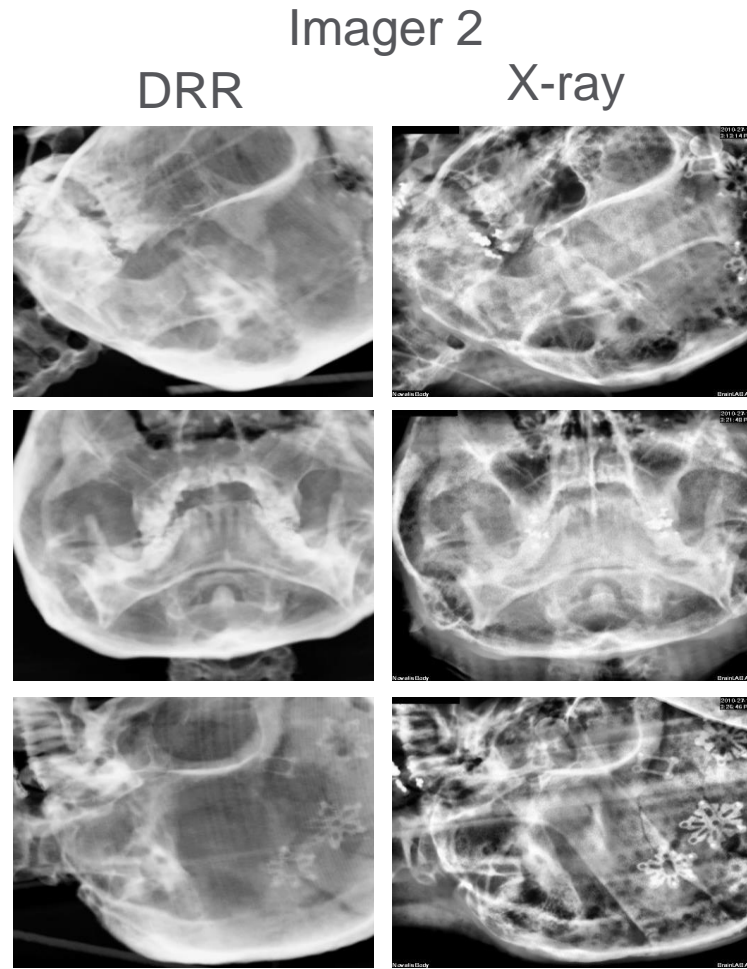
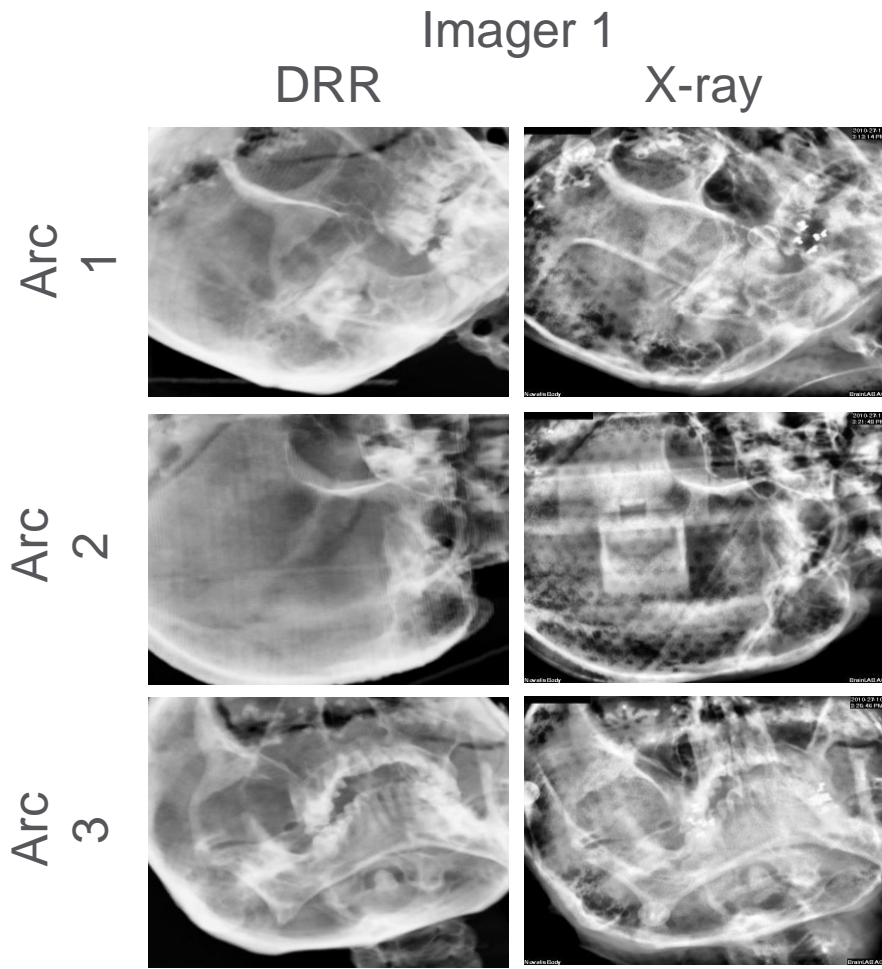


# EXACTRAC X-RAY



# EXACTRAC X-RAY

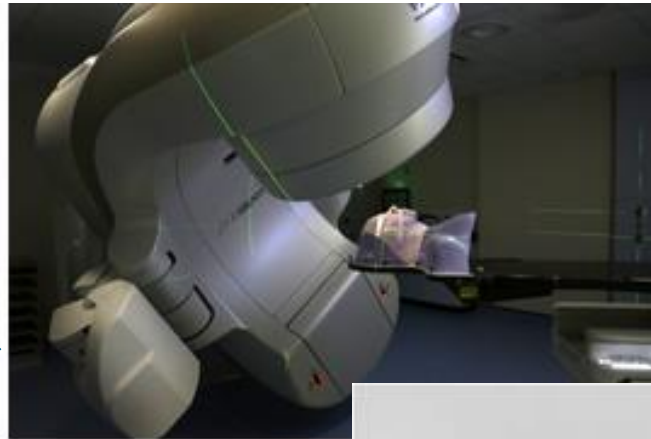
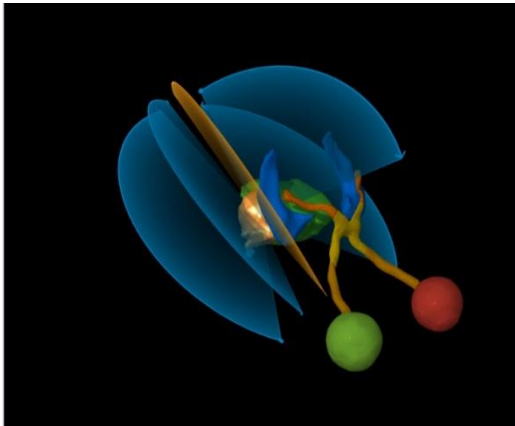
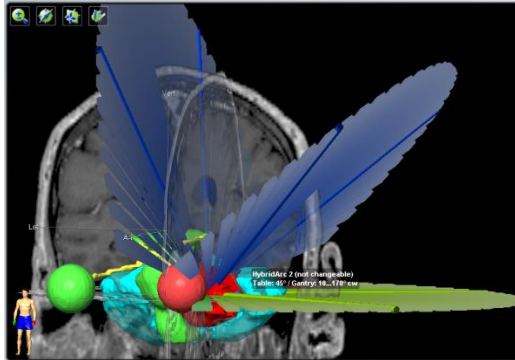
## NON-COPLANAR IMAGE-GUIDED MONITORING



# EXACTRAC X-RAY

Distribuzione della dose per limitare la tossicità agli OAR ed ottimizzare CI

LINAC → tecnica ad archi non co-planari



GK → sorgenti multiple CO60



CK → linac based con reticolo di punti

[J Neurosurg](#). 2004 Nov;101 Suppl 3:351-5

### Geometrical accuracy of the Novalis stereotactic radiosurgery system for trigeminal neuralgia.

•[Rahimian J](#)<sup>1</sup>, [Chen JC](#), [Rao AA](#), [Girvigian MR](#), [Miller MJ](#), [Greathouse HE](#).

#### Author information

<sup>1</sup>Departments of Radiation Oncology and Neurological Surgery, Southern California Permanente Medical Group, Los Angeles, 90027, USA. Javad.X.Rahimian@KP.org

#### Abstract

##### OBJECT:

Stringent geometrical accuracy and precision are required in the stereotactic radiosurgical treatment of patients. Accurate targeting is especially important when treating a patient in a single fraction of a very high radiation dose (90 Gy) to a small target such as that used in the treatment of trigeminal neuralgia (3 to 4-mm diameter). The purpose of this study was to determine the inaccuracies in each step of the procedure including imaging, fusion, treatment planning, and finally the treatment. The authors implemented a detailed quality-assurance program.

##### METHODS:

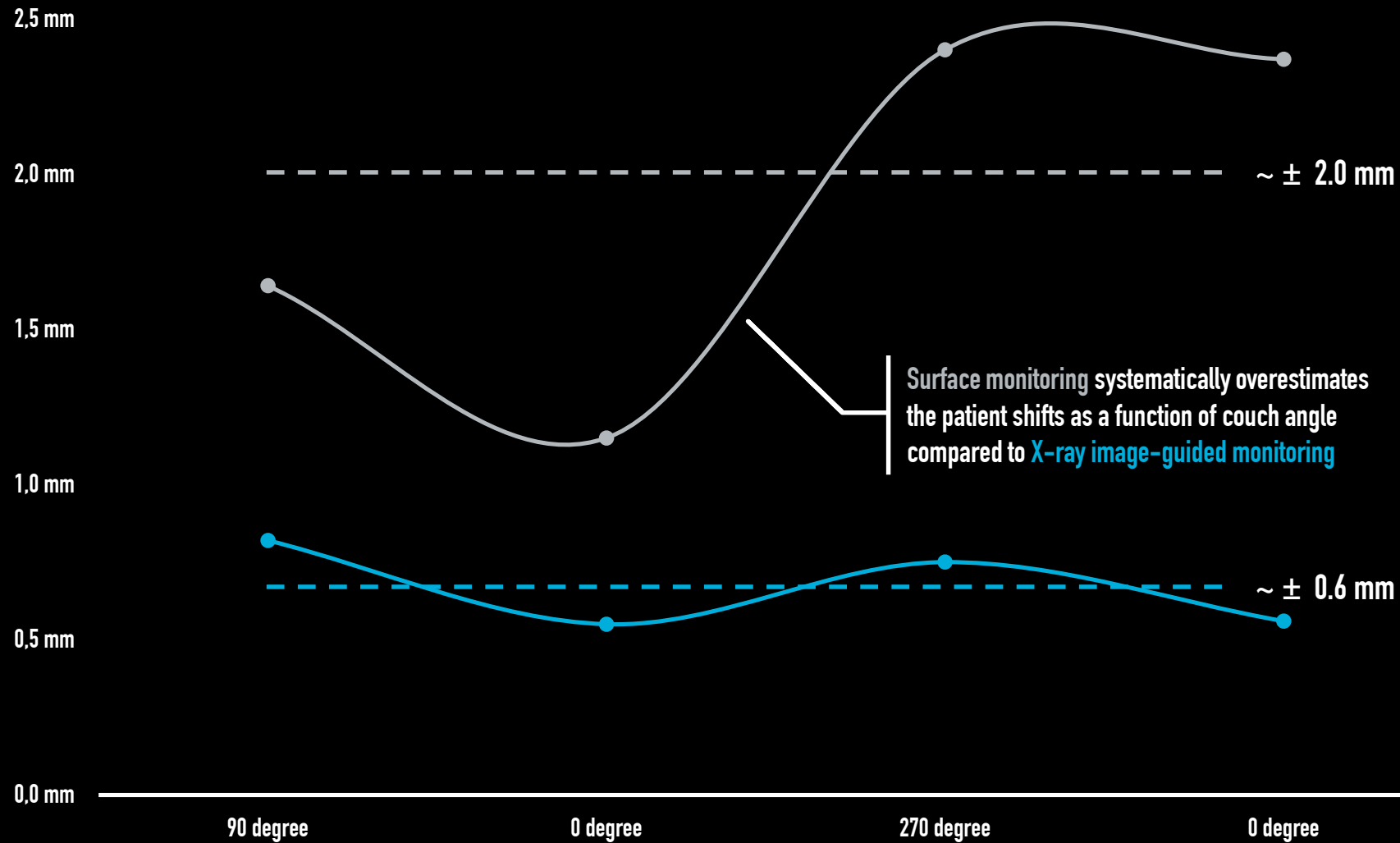
Overall geometrical accuracy of the Novalis stereotactic system was evaluated using a Radionics Geometric Phantom Chamber. The phantom has several magnetic resonance (MR) and computerized tomography (CT) imaging-friendly objects of various shapes and sizes. Axial 1-mm-thick MR and CT images of the phantom were acquired using a T1-weighted three-dimensional spoiled gradient recalled pulse sequence and the CT scanning protocols used clinically in patients. The absolute errors due to MR image distortion, CT scan resolution, and the image fusion inaccuracies were measured knowing the exact physical dimensions of the objects in the phantom. The isocentric accuracy of the Novalis gantry and the patient support system was measured using the Winston-Lutz test. Because inaccuracies are cumulative, to calculate the system's overall spatial accuracy, the root mean square (RMS) of all the errors was calculated. To validate the accuracy of the technique, a 1.5-mm-diameter spherical marker taped on top of a radiochromic film was fixed parallel to the x-z plane of the stereotactic coordinate system inside the phantom. The marker was defined as a target on the CT images, and seven noncoplanar circular arcs were used to treat the target on the film. The calculated system RMS value was then correlated with the position of the target and the highest density on the radiochromic film. The mean spatial errors due to image fusion and MR imaging were 0.41 $\pm$ 0.3 and 0.22 $\pm$ 0.1 mm, respectively. Gantry and couch isocentricities were 0.3 $\pm$ 0.1 and 0.6 $\pm$ 0.15 mm, respectively. The system overall RMS values were 0.9 and 0.6 mm with and without the couch errors included, respectively (isocenter variations due to couch rotation are microadjusted between couch positions). The positional verification of the marker was within 0.7 $\pm$ 0.1 mm of the highest optical density on the radiochromic film, correlating well with the system's overall RMS value. The overall mean system deviation was 0.32 $\pm$ 0.42 mm.

##### CONCLUSIONS:

The highest spatial errors were caused by image fusion and gantry rotation. A comprehensive quality-assurance program was developed for the authors' stereotactic radiosurgery program that includes medical imaging, linear accelerator mechanical isocentricity, and treatment delivery. For a successful treatment of trigeminal neuralgia with a 4-mm cone, the overall RMS value of equal to or less than 1 mm must be guaranteed.

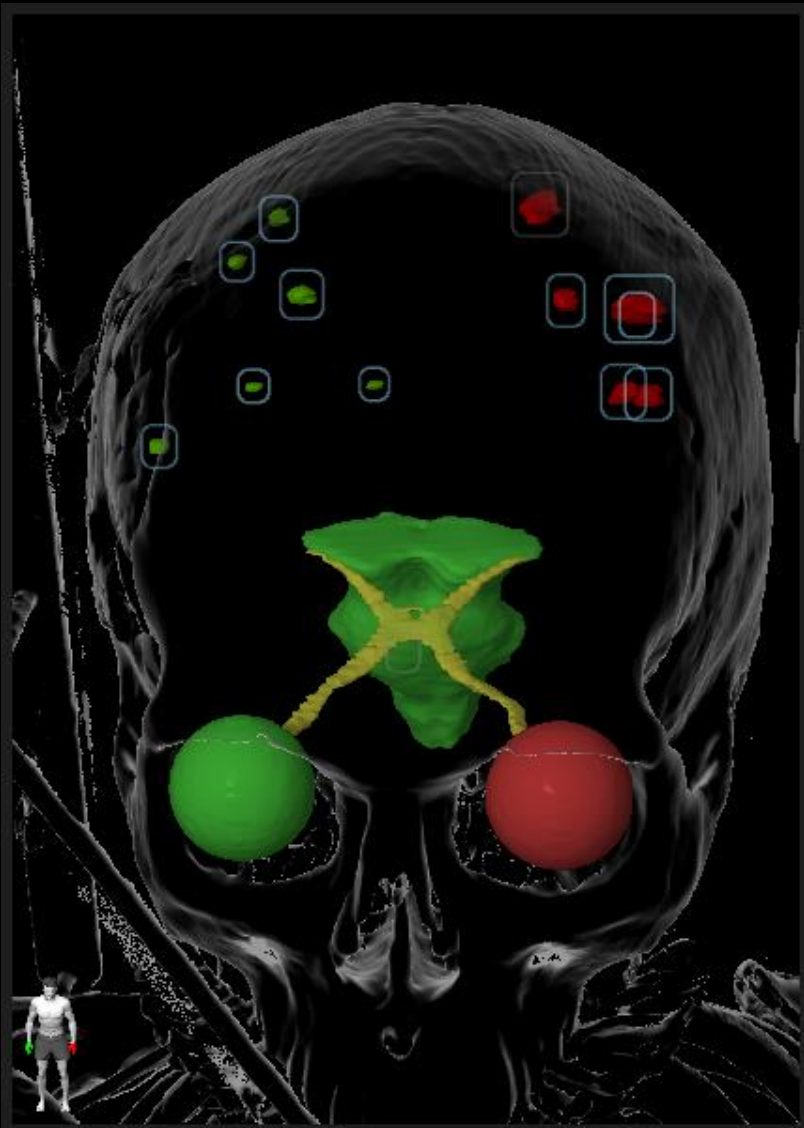


# EXACTRAC PROPOSITION SUPERIOR MONITORING ACCURACY



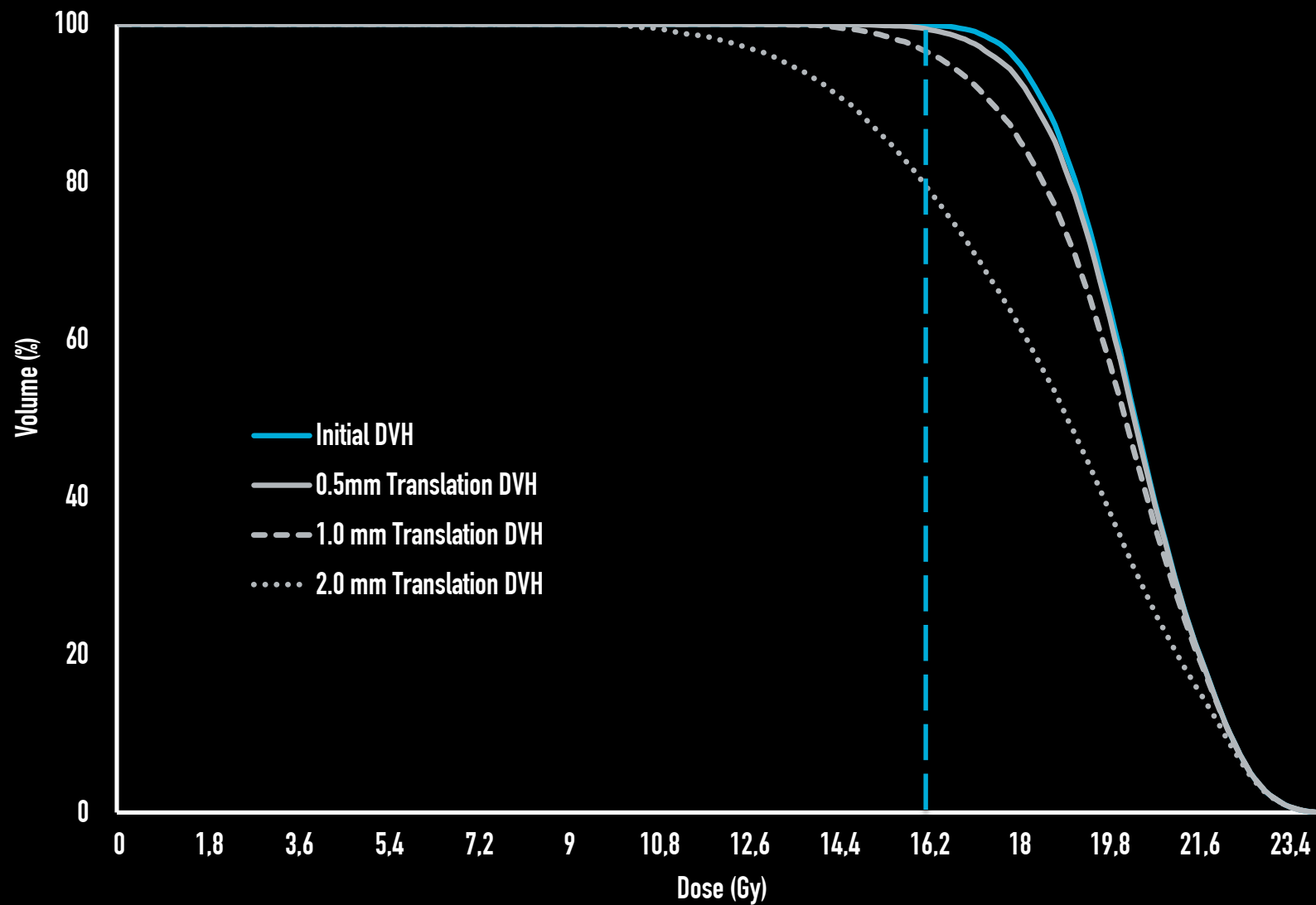
# DOSIMETRIC IMPACT OF REMAINING ROTATIONS

## EXAMPLE OF A THIRTEEN BRAIN METASTASES CASE



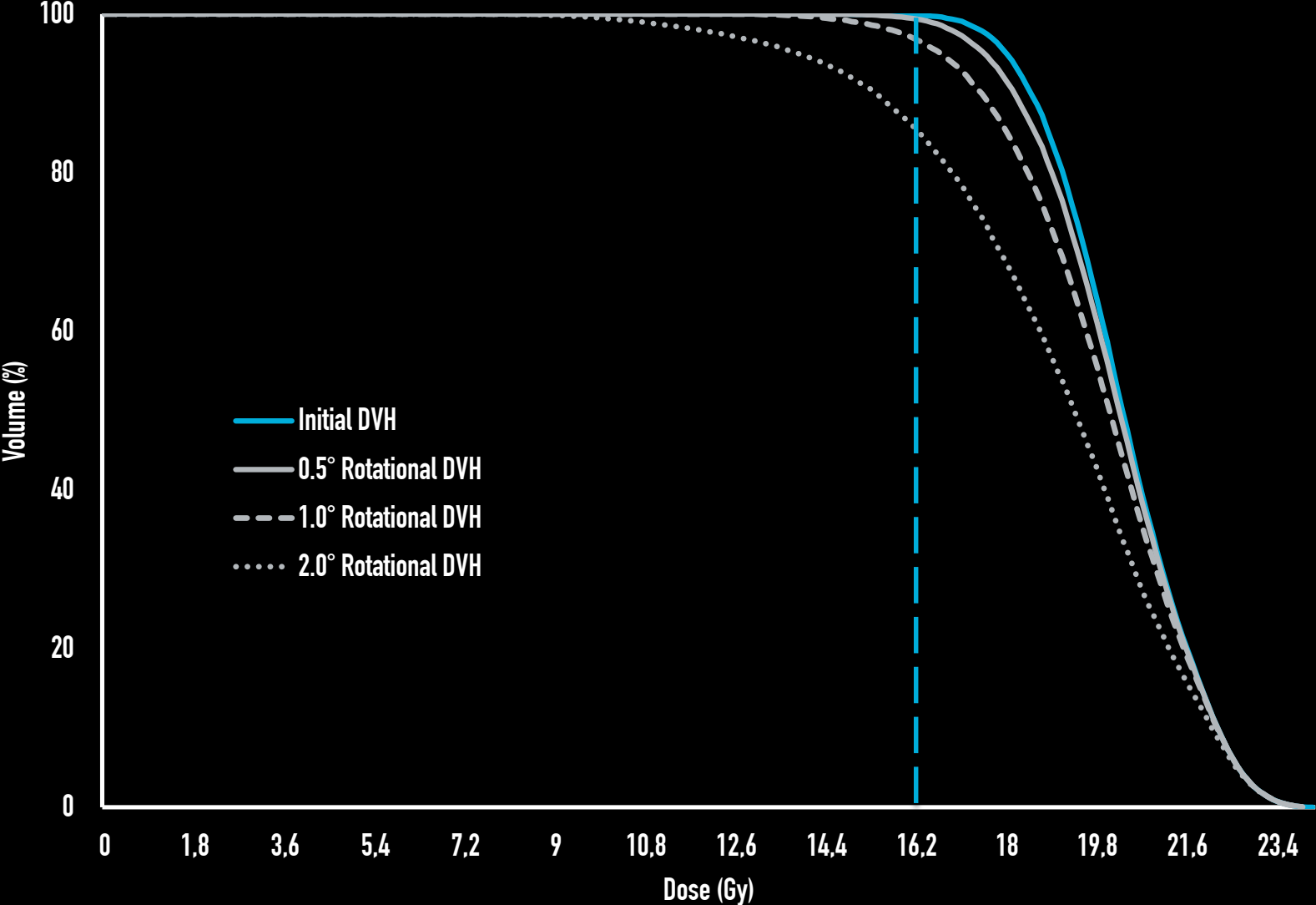
# DVH ANALYSIS

## TRANSLATIONAL DEVIATIONS



# DVH ANALYSIS

## ROTATIONAL DEVIATIONS



## Accuracy of surface registration compared to conventional volumetric registration in patient positioning for head-and-neck radiotherapy: A simulation study using patient data

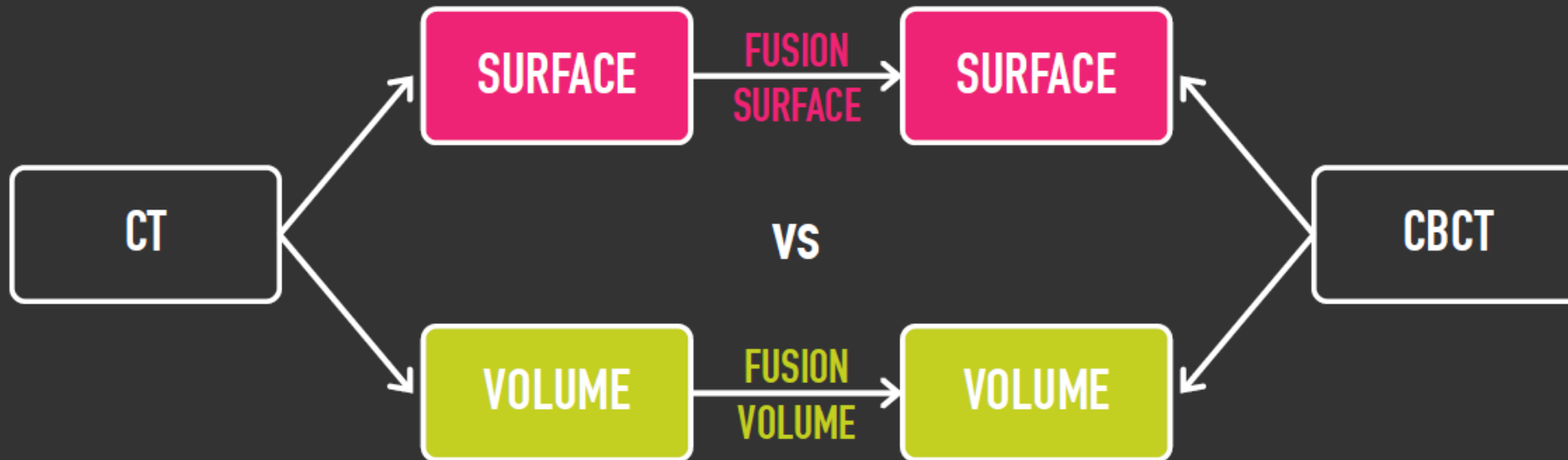
[Youngjun Kim](#)<sup>1</sup>, [Ruijiang Li](#)<sup>2</sup>, [Yong Hum Na](#)<sup>2</sup>, [Rena Lee](#)<sup>3,a)</sup> and [Lei Xing](#)<sup>4</sup>

- Purpose: 3D optical surface imaging has been applied to patient positioning in radiation therapy (RT). The optical patient positioning system is advantageous over conventional method using cone-beam computed tomography (CBCT) in that it is radiation free, frameless, and is capable of real-time monitoring. While the conventional radiographic method uses volumetric registration, the optical system uses surface matching for patient alignment. The relative accuracy of these two methods has not yet been sufficiently investigated. This study aims to investigate the theoretical accuracy of the surface registration based on a simulation study using patient data.
- Methods: This study compares the relative accuracy of surface and volumetric registration in head-and-neck RT. The authors examined 26 patient data sets, each consisting of planning CT data acquired before treatment and patient setup CBCT data acquired at the time of treatment. As input data of surface registration, patient's skin surfaces were created by contouring patient skin from planning CT and treatment CBCT. Surface registration was performed using the iterative closest points algorithm by point-plane closest, which minimizes the normal distance between source points and target surfaces. Six degrees of freedom (three translations and three rotations) were used in both surface and volumetric registrations and the results were compared. The accuracy of each method was estimated by digital phantom tests.
- Results: Based on the results of 26 patients, the authors found that the average and maximum root-mean-square translation deviation between the surface and volumetric registrations were 2.7 and 5.2 mm, respectively. The residual error of the surface registration was calculated to have an average of 0.9 mm and a maximum of 1.7 mm.
- Conclusions: Surface registration may lead to results different from those of the conventional volumetric registration. Only limited accuracy can be achieved for patient positioning with an approach based solely on surface information.

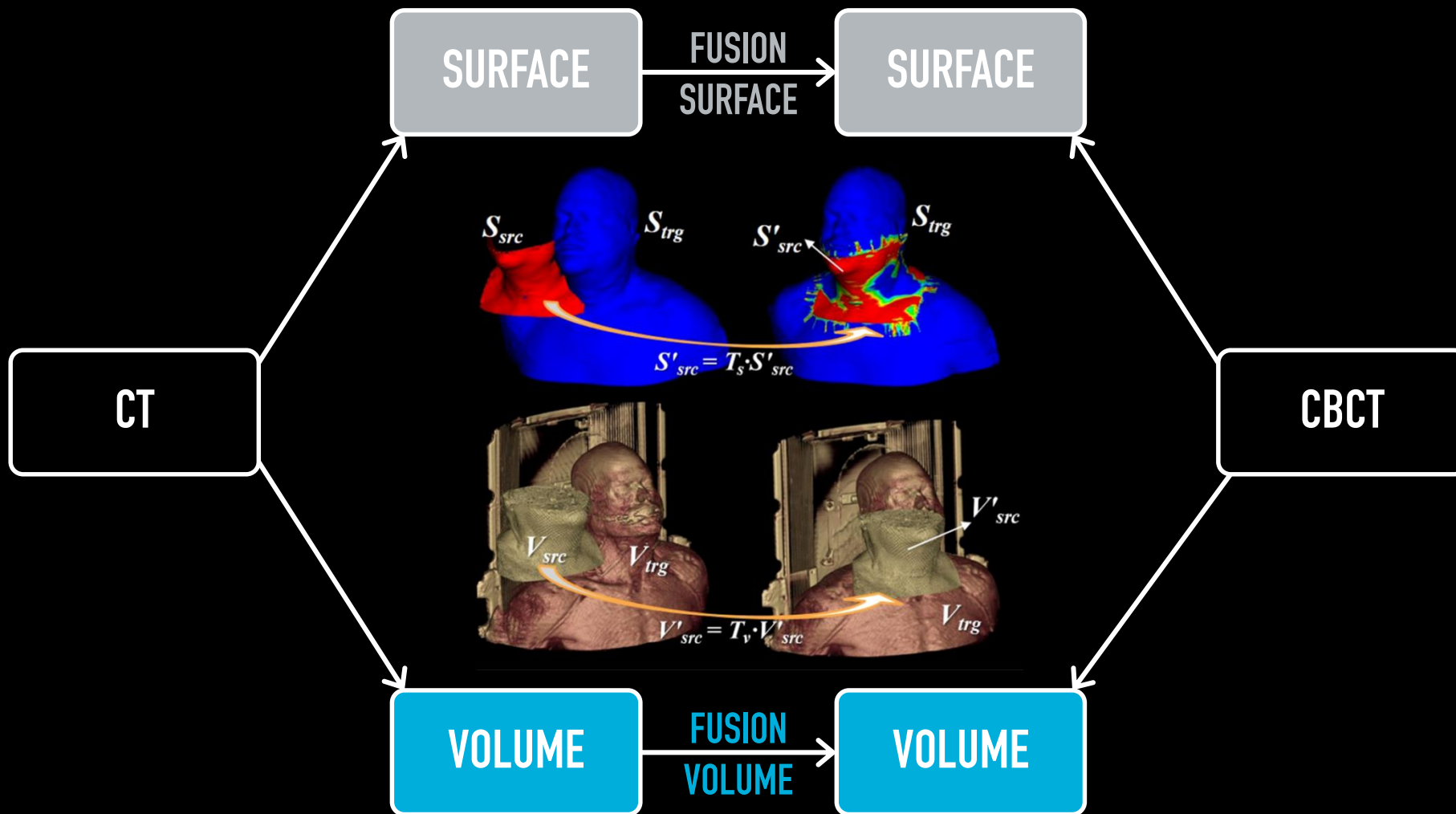
Accuracy of **surface registration** compared to conventional **volumetric registration** in patient positioning for head-and-neck radiotherapy:  
A simulation study using patient data.



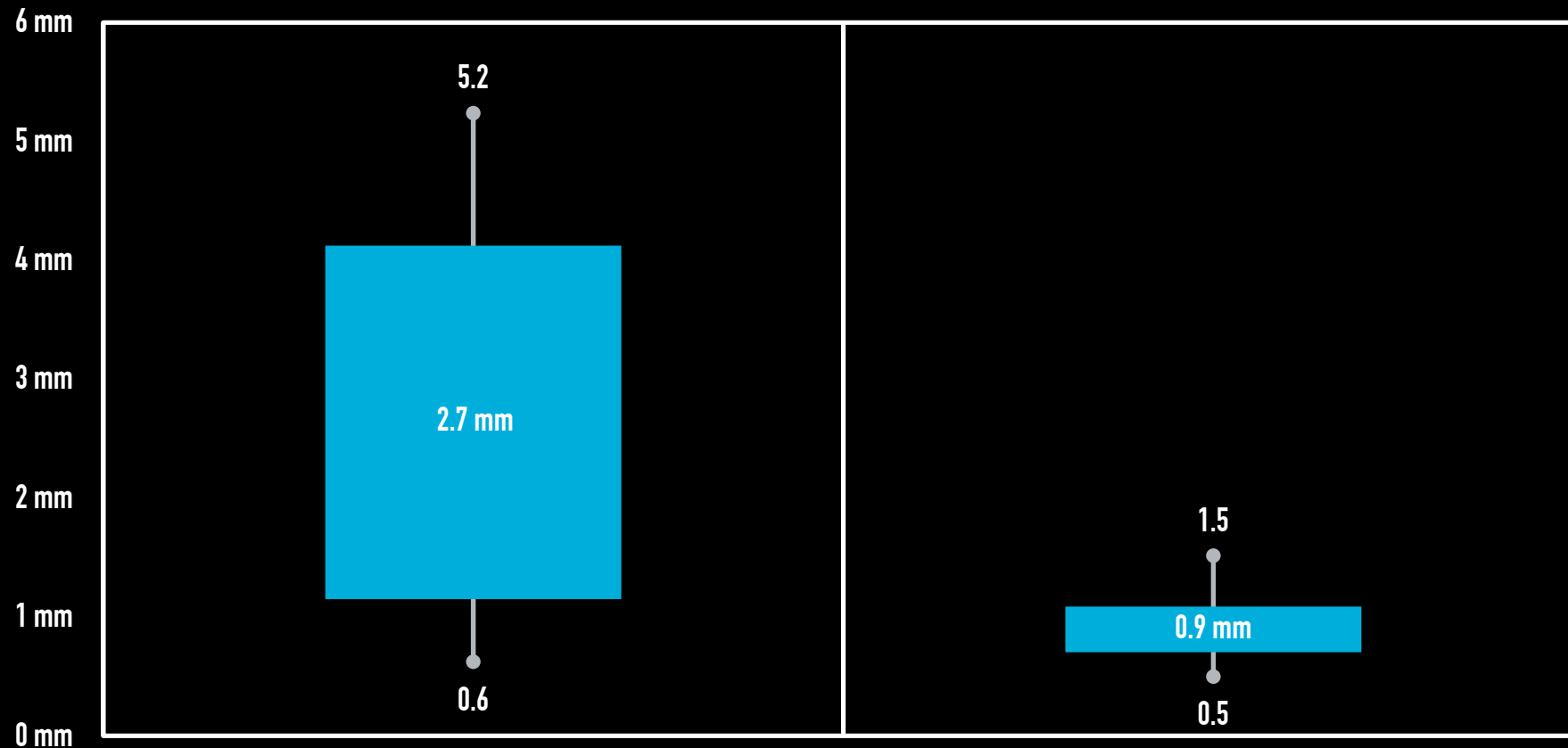
26 H&N Patients  
Retrospective analysis  
Varian TrueBeam Linac  
Stanford School of Medicine



# EXACTRAC PROPOSITION SUPERIOR MONITORING ACCURACY



# EXACTRAC PROPOSITION SUPERIOR MONITORING ACCURACY



The mean and max total difference between both resulting transformation matrices underlying the respective fusions

Assessment of the accuracy of the iterative closest point (ICP) surface fusion algorithm by measuring the residual error



# EXACTRAC

## LINAC INDEPENDENT COMPATIBILITY

### State of the art Radiosurgery / IGRT system

- Two kV-X-Ray units recessed in the floor
- Two flat panels
- Integrated optical tracking system
- Dual X-Ray generator
- Proprietary 6D fusion

#### Top Indications

- Cranial
- Spine
- Lung
- Prostate
- Head and Neck



900+ systems in 49 countries

180,000 fractions per month

VARIAN



ELEKTA



## COMPATIBILITY WITH VARIAN PERFECTPITCH

- 6D positioning supported with ExacTrac 6.2



## COMPATIBILITY WITH ELEKTA

- Seamless integration of ExacTrac with Elekta linacs
- Automatic loading of the patient treatment plan to ExacTrac from MOSAIQ®
- Patient positioning in 6 degrees of freedom with HexaPOD™ evo RT system

# EXACTRAC

## OPTIONS



### FRAMELESS SRS



- Highly accurate delivery of single or multi-fraction SRS
- Rigid mask and fixation system

### POSITION PACKAGES



- Automated patient positioning
- Range of platforms (BL Robotics, Hexapod, Perfect Pitch)

### CBCT IMPORT AND ALIGNMENT



- Utilises CBCT data to allow soft tissue set up

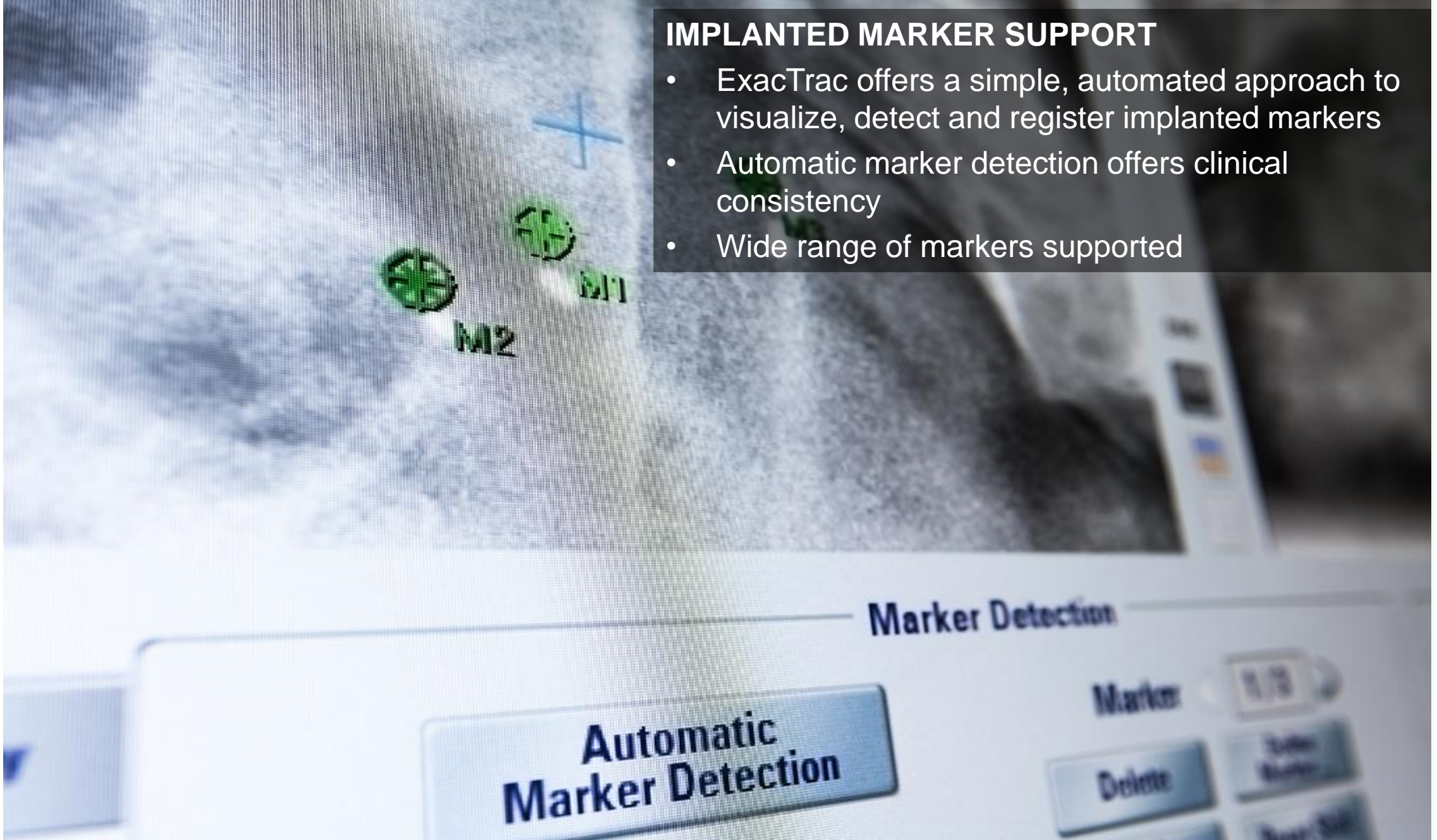
### IMPLANTED MARKER TRACKING



- Simple and automated approach to visualise and detect implanted markers
- Wide range of implanted markers supported

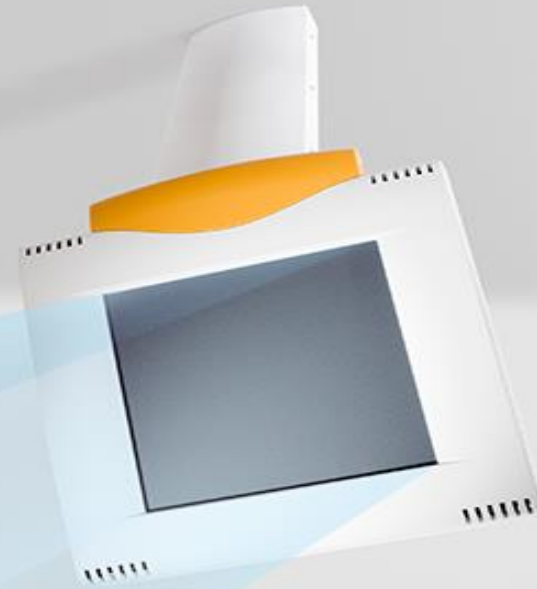
## IMPLANTED MARKER SUPPORT

- ExacTrac offers a simple, automated approach to visualize, detect and register implanted markers
- Automatic marker detection offers clinical consistency
- Wide range of markers supported



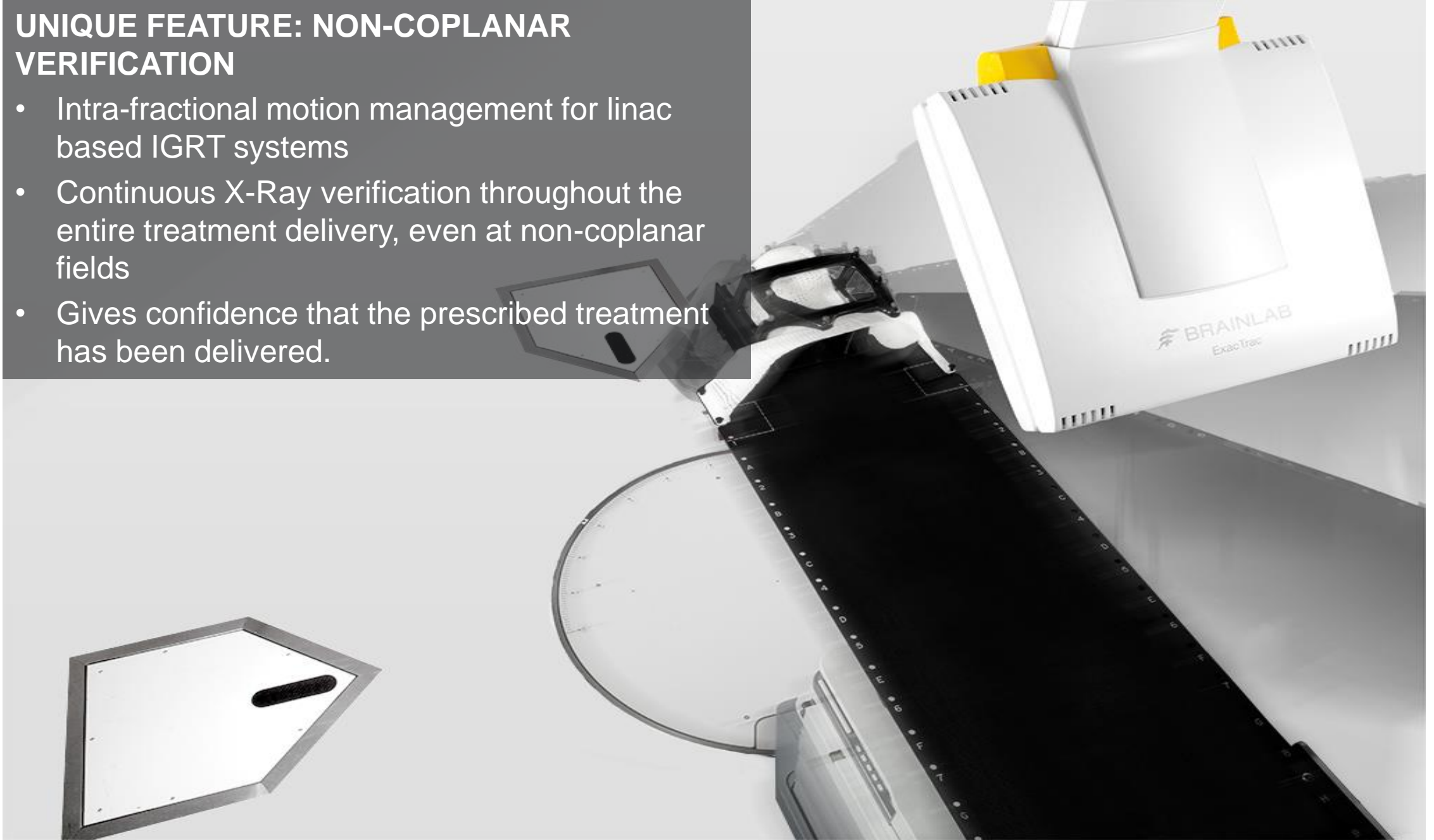
## FRAMELESS CRANIAL RADIOSURGERY

- Highly accurate delivery of single or multi-fraction treatment
- Precise non-invasive stereotactic mask system designed for re-producible conformity
- Streamlined workflow overcomes the restrictions of frame based radiosurgery



## UNIQUE FEATURE: NON-COPLANAR VERIFICATION

- Intra-fractional motion management for linac based IGRT systems
- Continuous X-Ray verification throughout the entire treatment delivery, even at non-coplanar fields
- Gives confidence that the prescribed treatment has been delivered.





THANK  
YOU

[pier.raguzzi@brainlab.com](mailto:pier.raguzzi@brainlab.com)